

Breast cancer research with a novel molecular imaging diagnostic system

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*15th Workshop on European Collaboration in
Higher Education on Radiological and Nuclear
Engineering and Radiation Protection*

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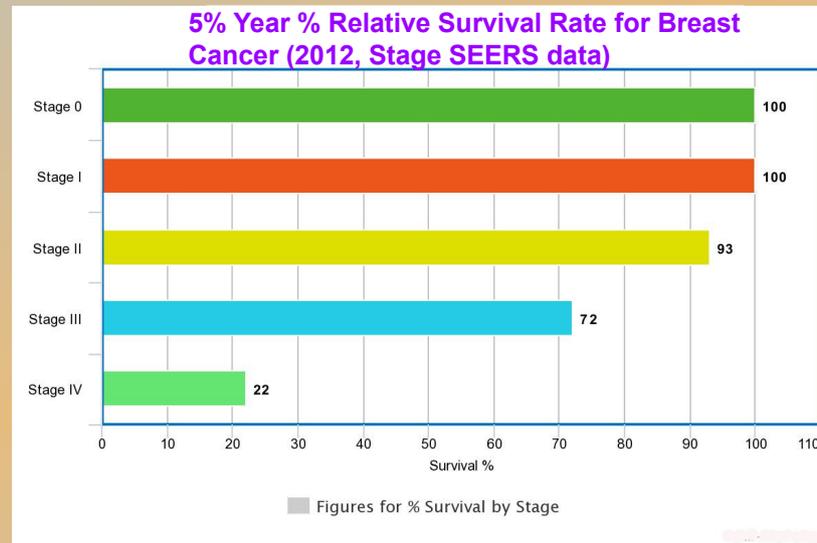
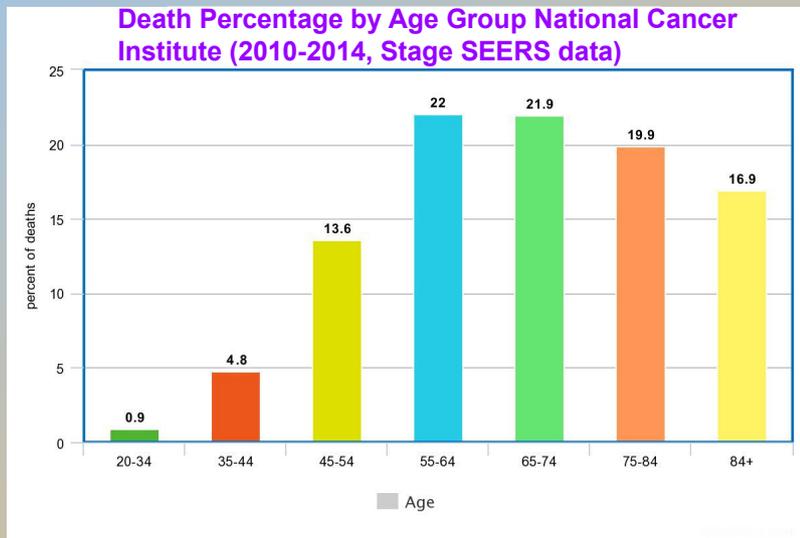
Outline

- ✓ Breast Cancer Statistics
- ✓ Breast Imaging: techniques, features & issues
- ✓ Molecular Breast Imaging System
- ✓ A novel MBI system prototype with two asymmetrical heads

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- ✓ Molecular Breast Imaging System
- ✓ A novel MBI system prototype with two asymmetrical heads
- ✓ Characterization and Calibration Campaigns
- ✓ Angular Identification of lesion: LAT configuration
- ✓ Simulation tool: GATE software
- ✓ Spot-compression configuration: real-simulated data comparison

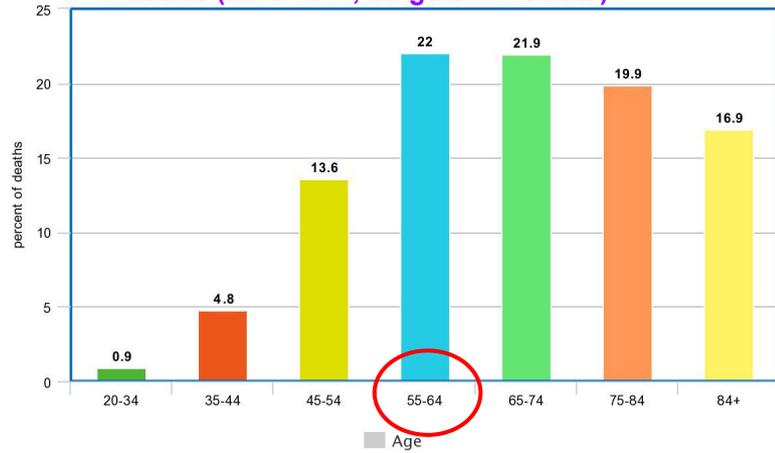
Breast Cancer Statistics



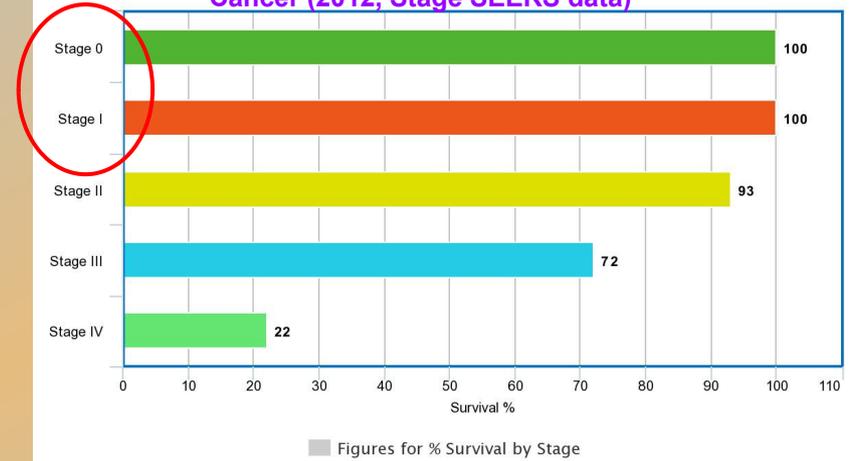
- 1st Women Cancer, 2nd for Death
- Sites: lympho nodes, ducts, lobules
BIRADS classes: 0 to 6
(100% malignancy)

Breast Cancer Statistics

Death Percentage by Age Group National Cancer Institute (2010-2014, Stage SEERS data)

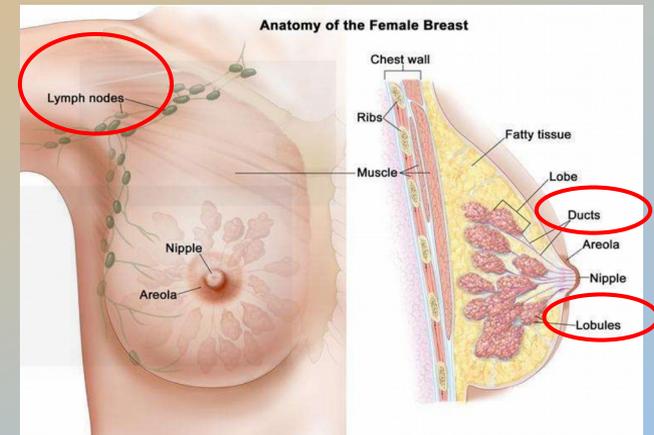
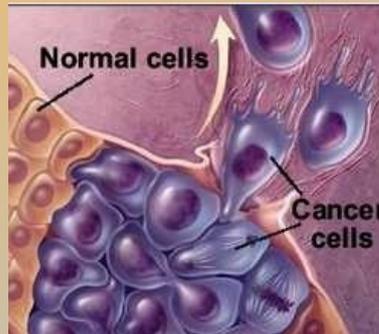


5% Year % Relative Survival Rate for Breast Cancer (2012, Stage SEERS data)



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Breast Imaging: features & issues

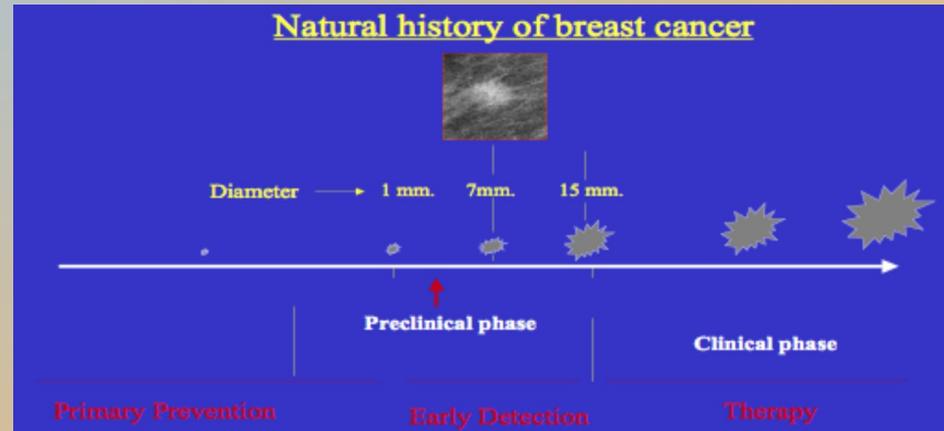
Three-step Diagnosis

- Clinical Evaluation
- **Imaging**
- Biopsy

Breast Imaging: features & issues

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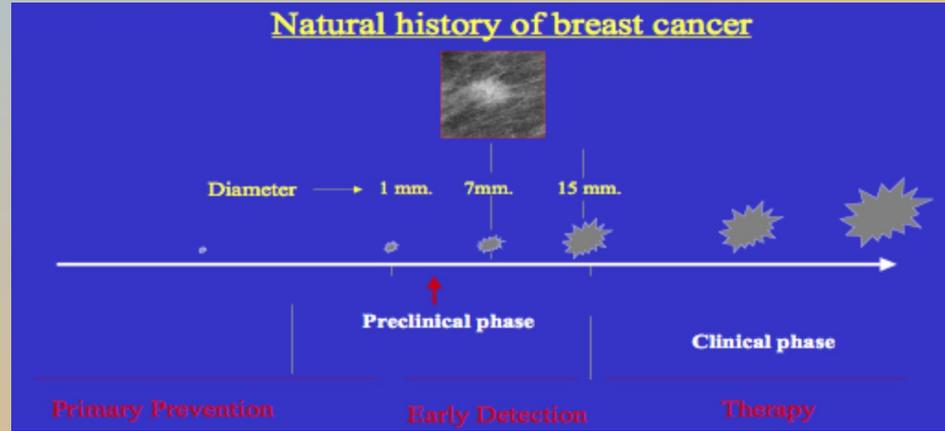


**Early diagnosis,
in preclinical
phase
($<10\text{mm}$, $\sim 5\text{mm}$)**

Breast Imaging: features & issues

Three-step Diagnosis

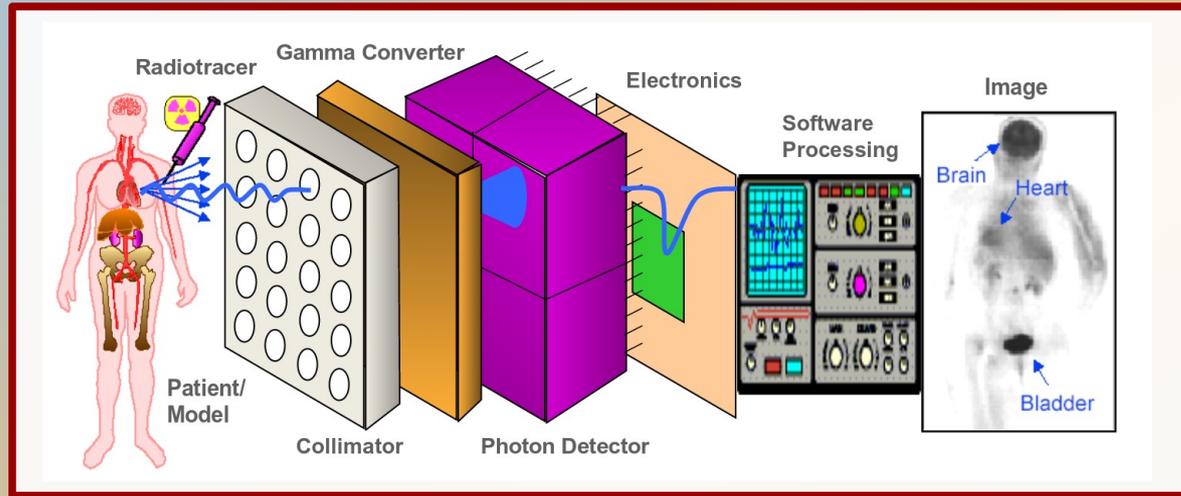
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Early diagnosis, in preclinical phase (<10mm, ~5mm)

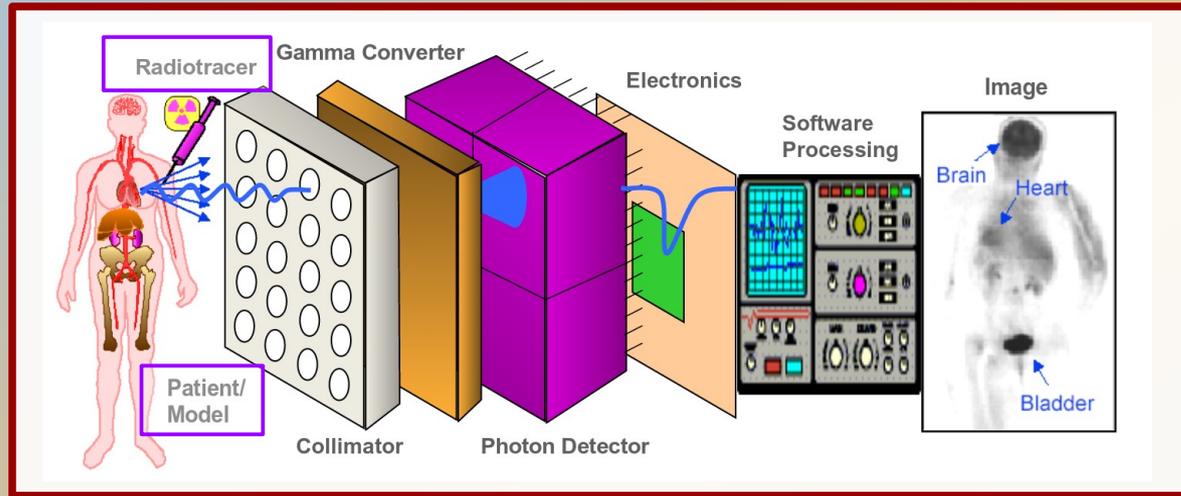
Param/Techn	MRx	US	MRI	PET	SPECT
Source	X-ray	Sound	e. m. wave	Single- γ	Double- γ
Imaging	Anatomical	Anatomical	Anatomical	Functional	Functional
Sensitivity	Medium	Medium	Medium-high	high	high
Specificity	high	low	Medium-high	high	medium
Limits	Dense Breast, FN rate	Attenuation, FN rate	Artifact, Costs, Time	Lifetime, Resolution	Statistics, Resolution

Molecular Breast Imaging System



Anger Camera scheme: single-head components

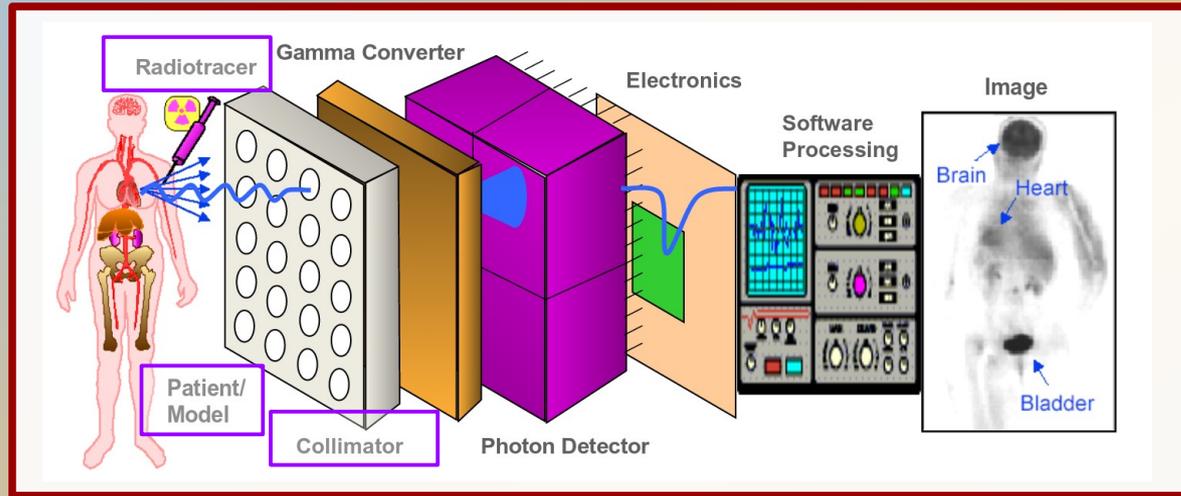
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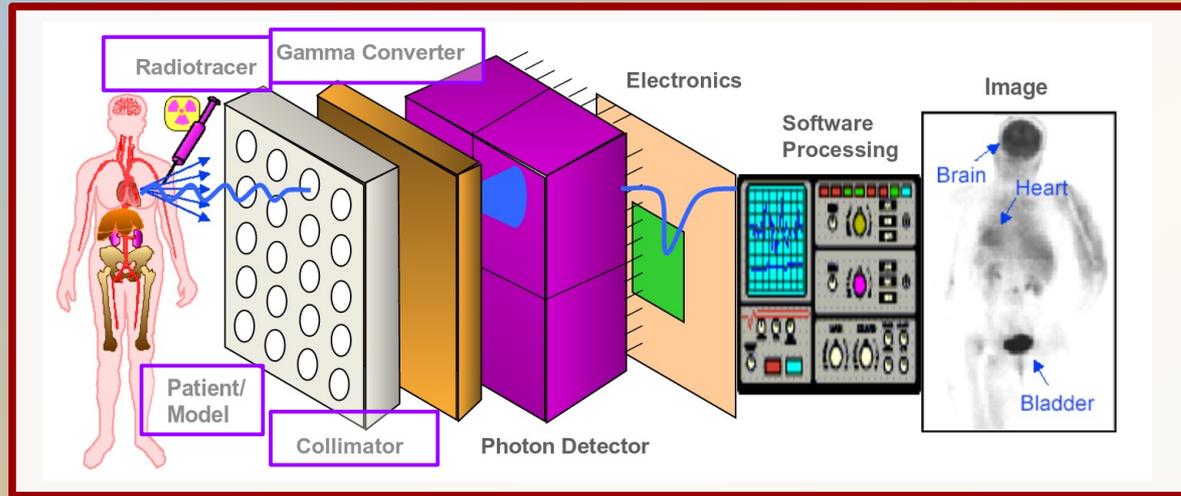
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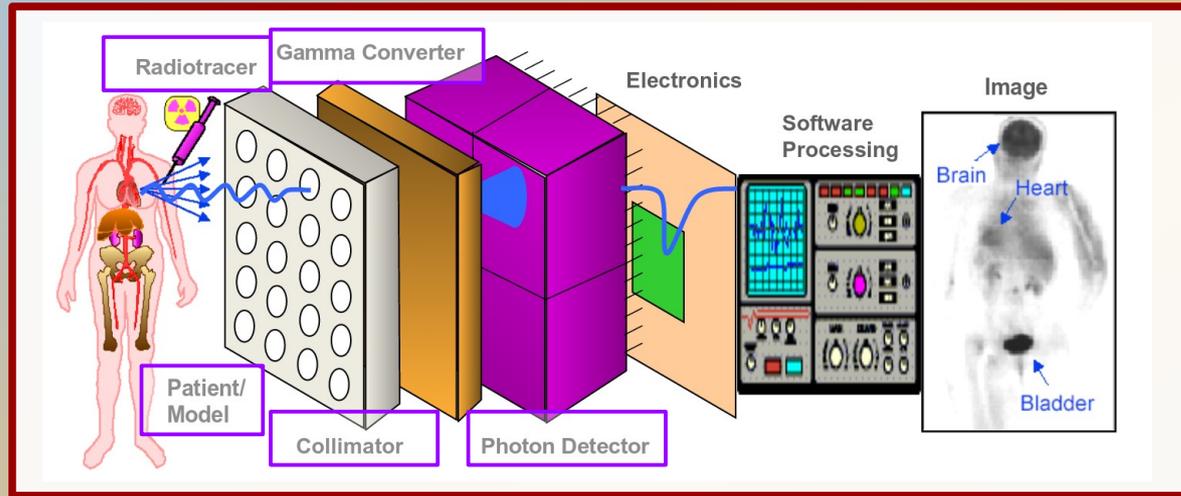
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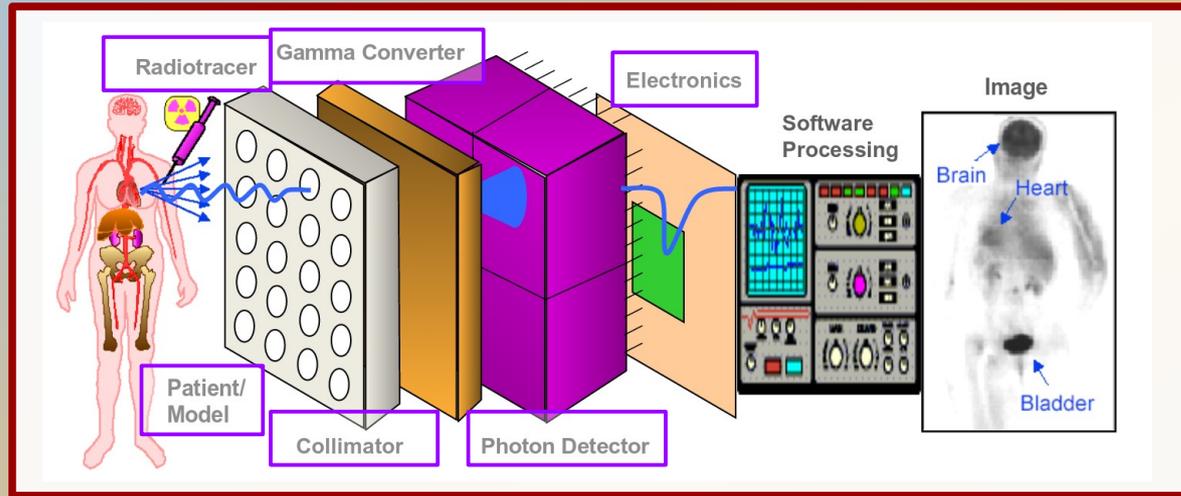


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- **Sensor:** converts light into electrical signals

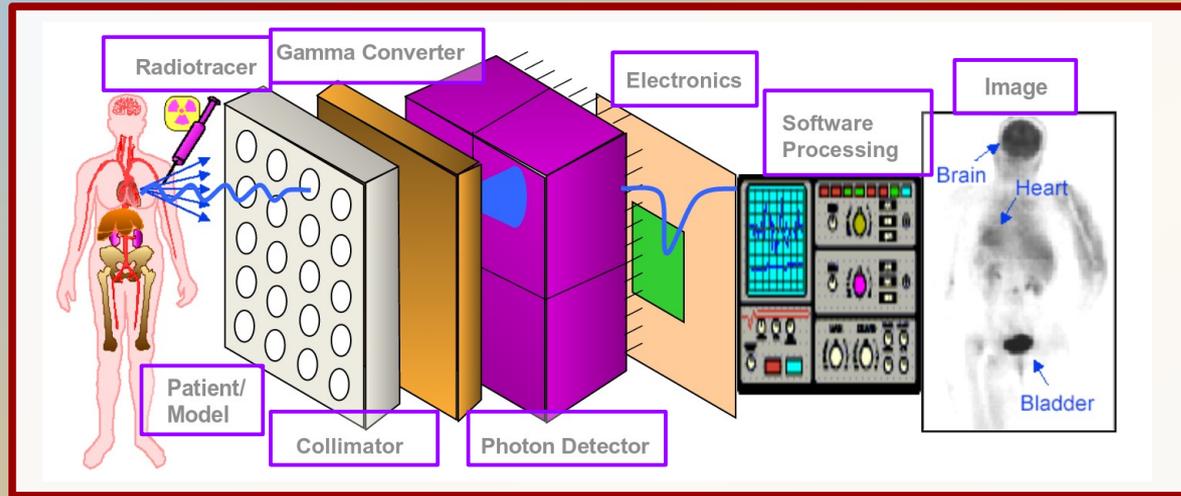
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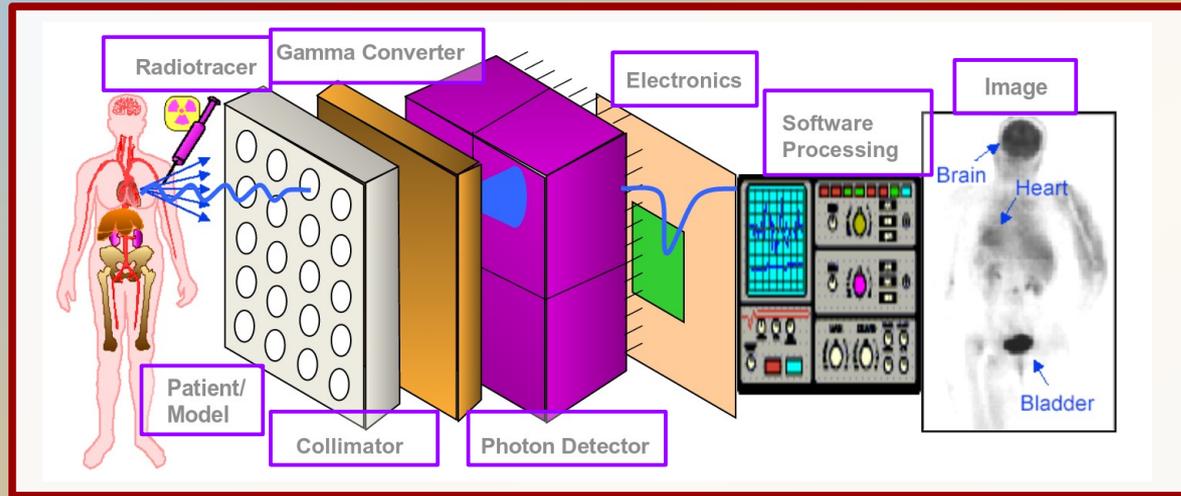
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Standard Gamma Camera Limit: unable to detect tumour < 10 mm

A novel MBI system prototype: two asymmetrical heads

Solution for detection of ≤ 5 mm tumour size:

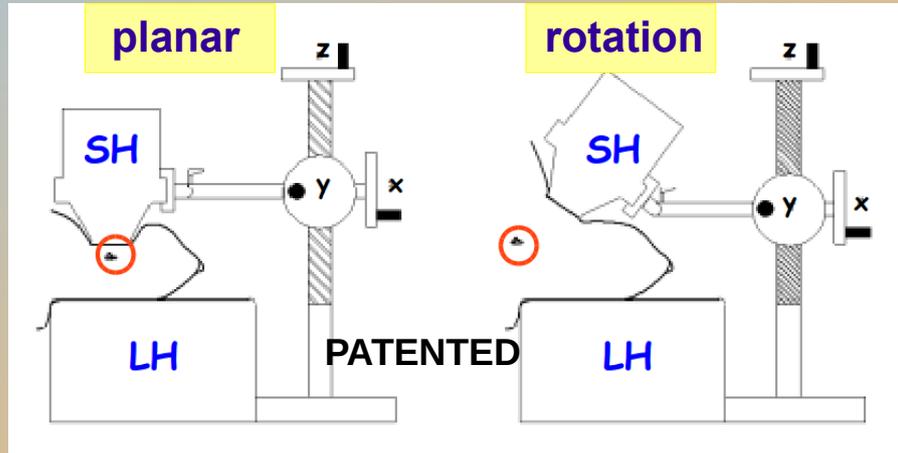
- high-efficiency & high-resolution, high sensibility, good energy resolution
- large head: parallel-holes optics, large field of view (breast support)
- small head points and zooms the lesion: pin-hole optics

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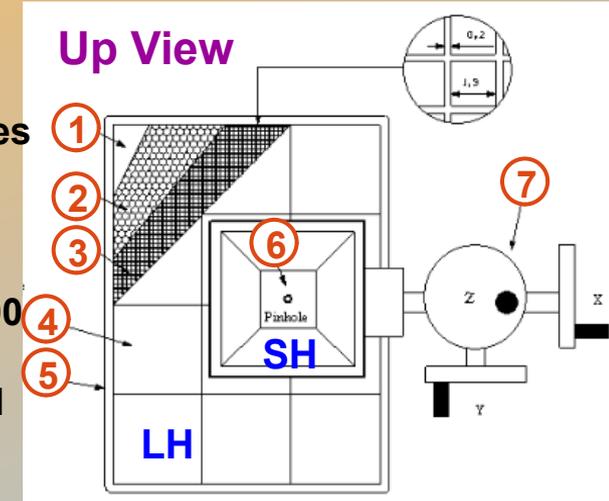
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Side View: breast compression



- ① Al foil 0.5 mm
- ② Parallel & hexagonal holes collimator, Pb
- ③ 150x200 mm² pixellated scintillator
- ④ PSPMT Hamamatsu 8500
- ⑤ External W box
- ⑥ Compressor small-head detector & pin-hole optic
- ⑦ Handling system

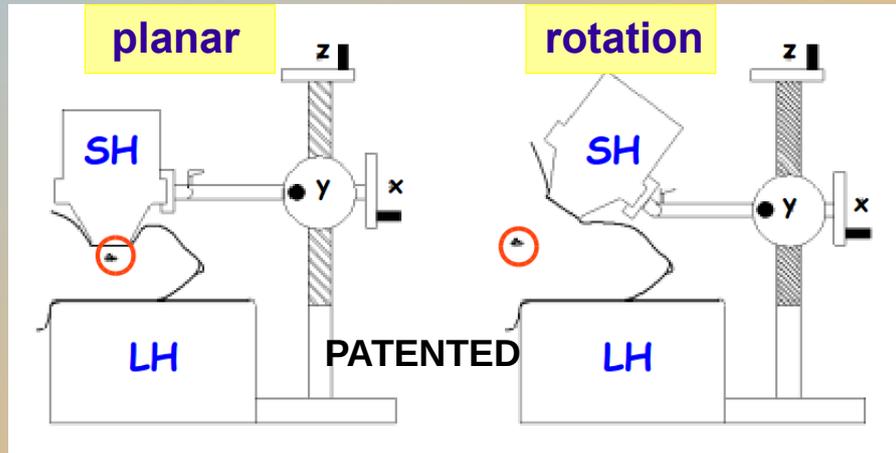


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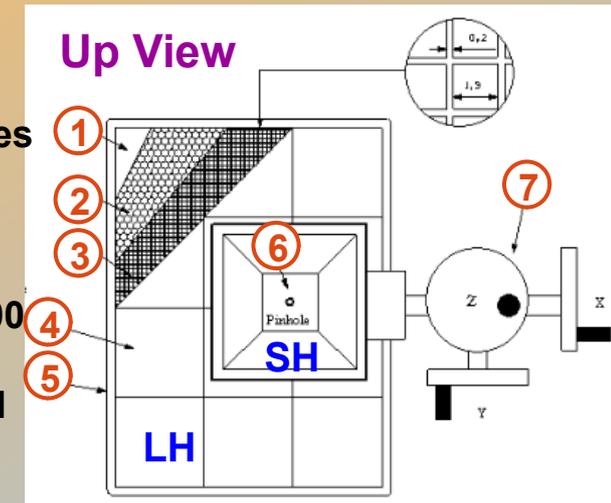
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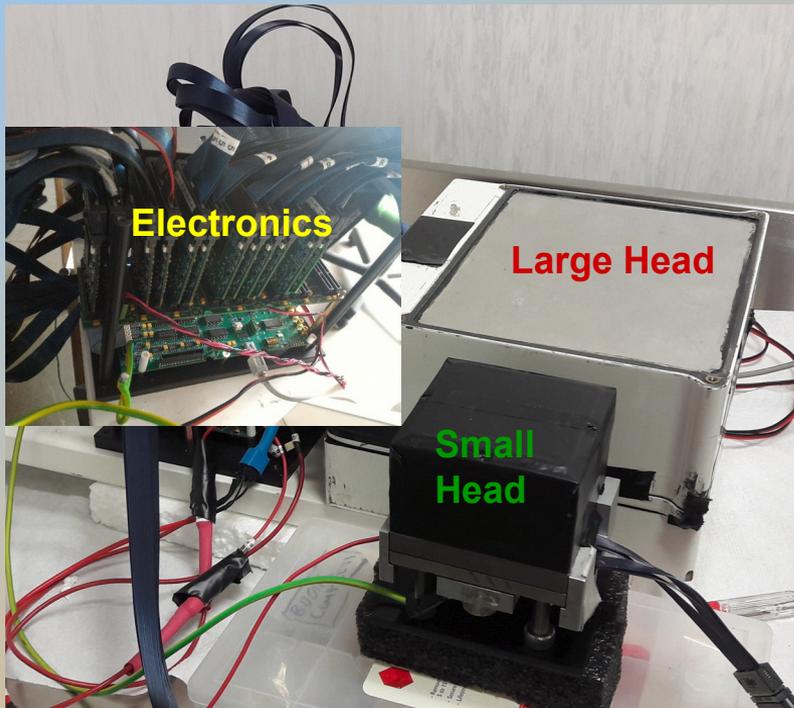


Detectability Key Parameters:

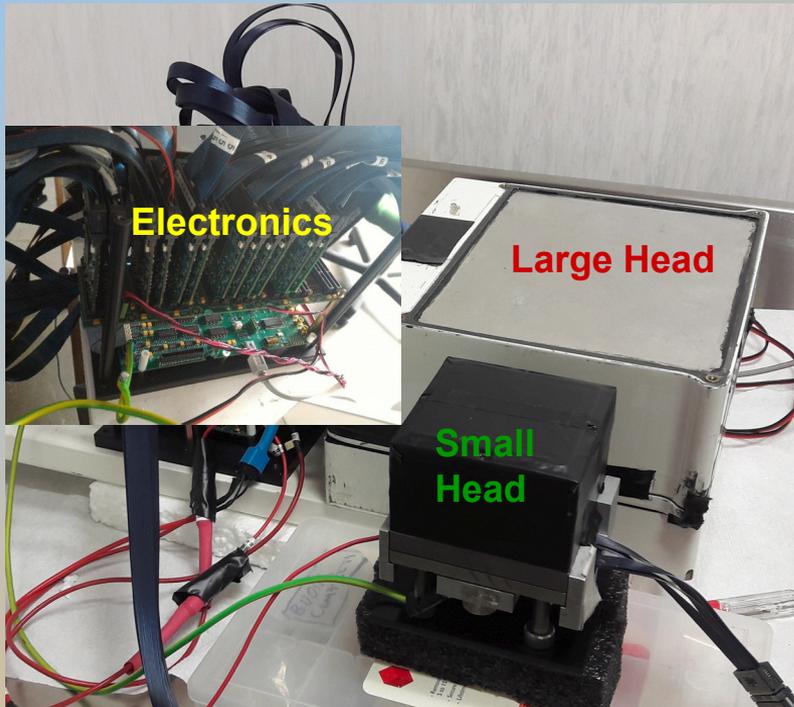
- SNR, CNR, spatial resolution
- Radiopharmaceutical Uptake

- Spot compression of SH & pinhole collimator → close to lesion, increasing efficiency & resolution (SNR & CNR) → detectability & image reconstruction → identification: planar & 3D

A novel MBI system prototype: components & features



A novel MBI system prototype: components & features

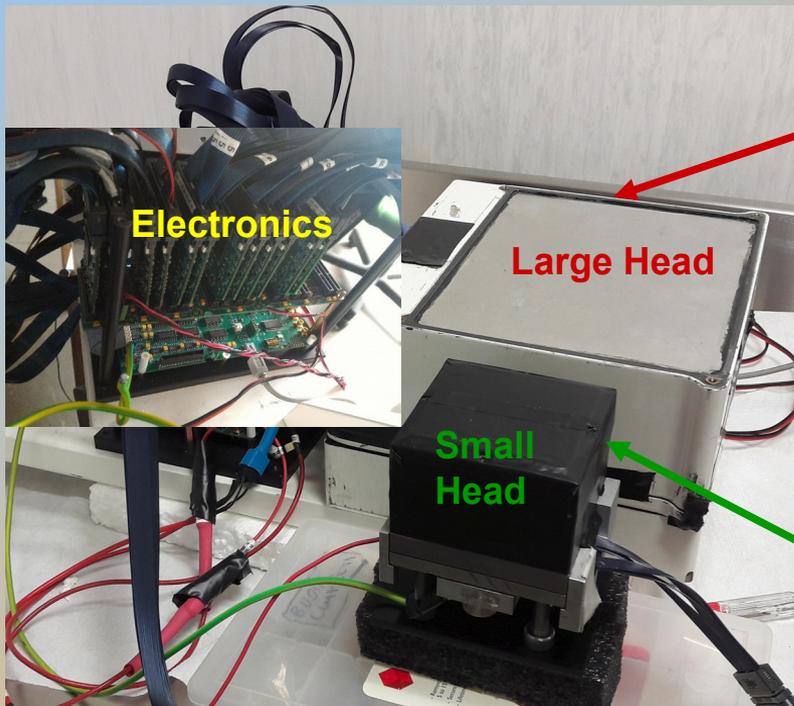


Electronics

Scintillators

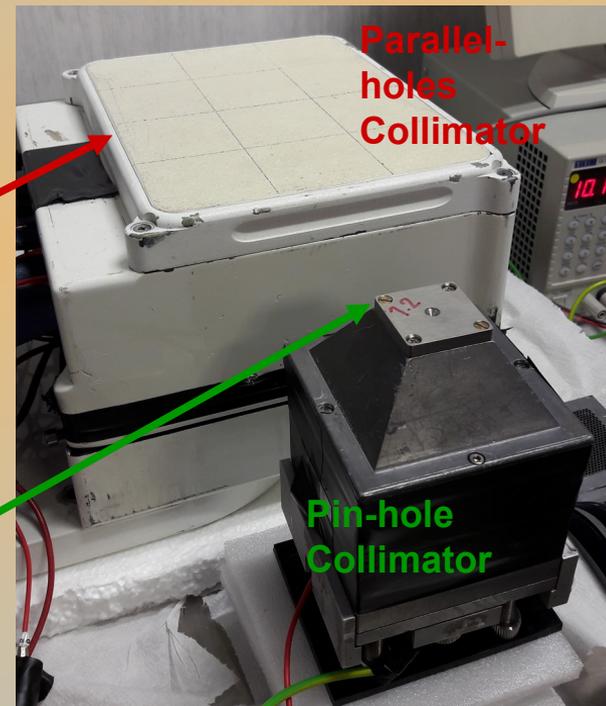
- Front End MAROC3 ASICs: up to 4096 independent channels
- FPGA based
- Thickness 0.5 mm
- Pixel size 1.3 ± 0.2 mm

A novel MBI system prototype: components & features



- 15x20 cm² size
- 3x4 PSPMT H8500 (6x6 mm²): 768 chs
- NaI(Tl) pixellated: 15x20 cm²
- Collimation: pitch 1.5 mm, 19 mm hexagonal septa; ≈ 3000 hole

- 5x5 cm² size
- 1 PSPMT H8500 64 chs
- NaI(Tl) pixellated: 5x5 cm²
- Collimation: 2 mm diam. size, ≈ 45 mm height

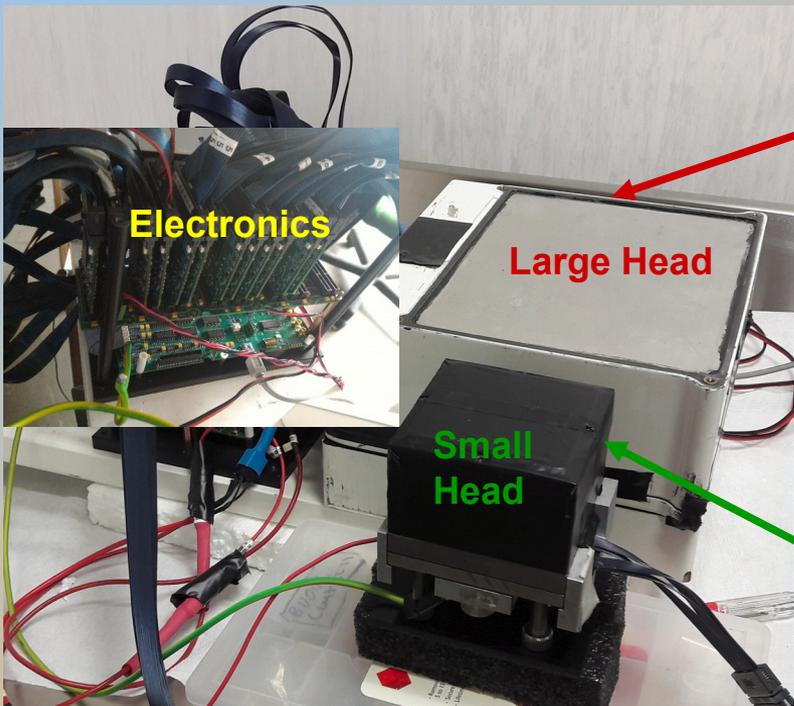


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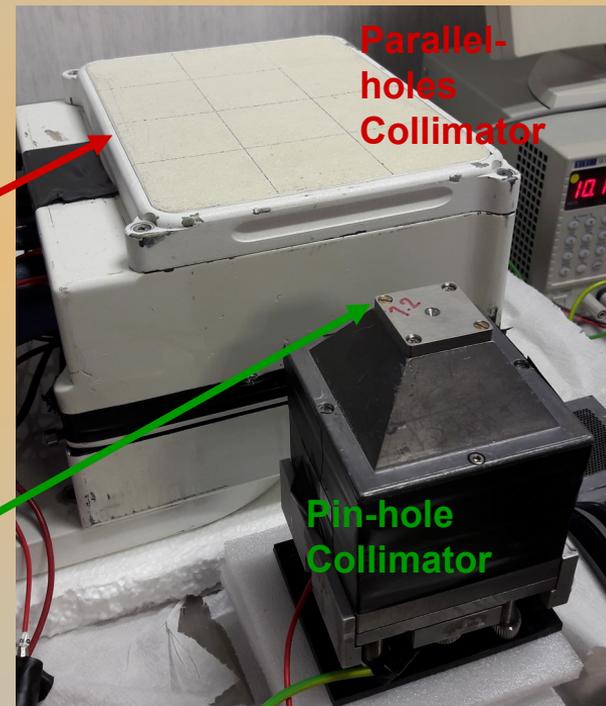
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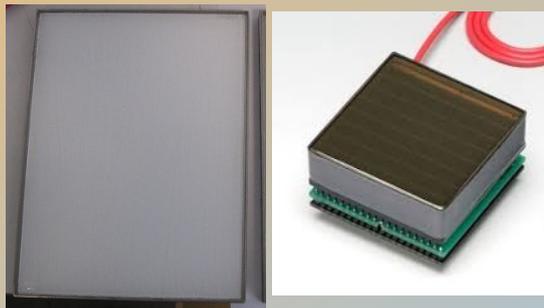


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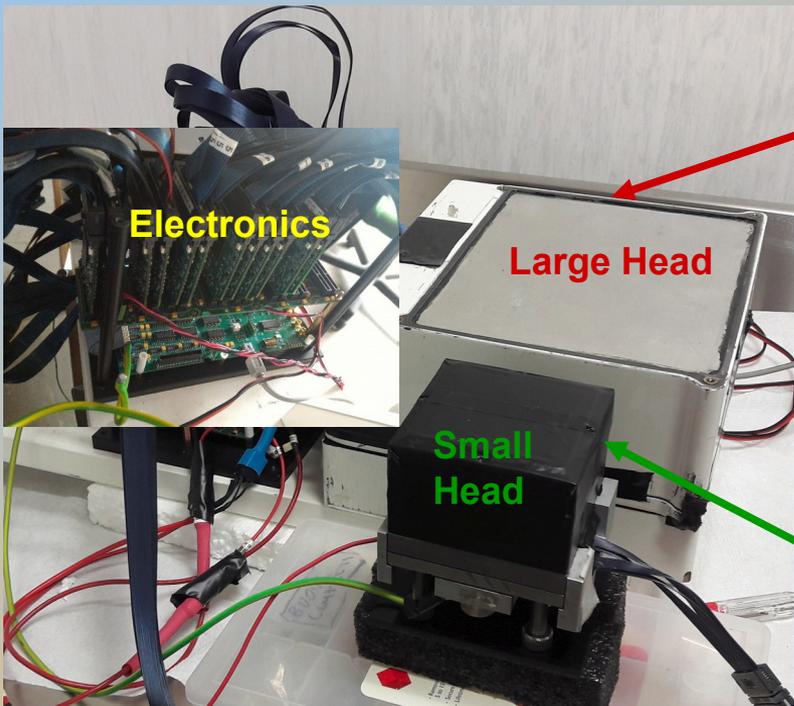
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Detectors

- Flat Panel PMT/H8500 64chs
- Anode size/pitch: 5.8x5.8 /6.1 mm
- Gain max: 1.5x10⁶

A novel MBI system prototype: components & features



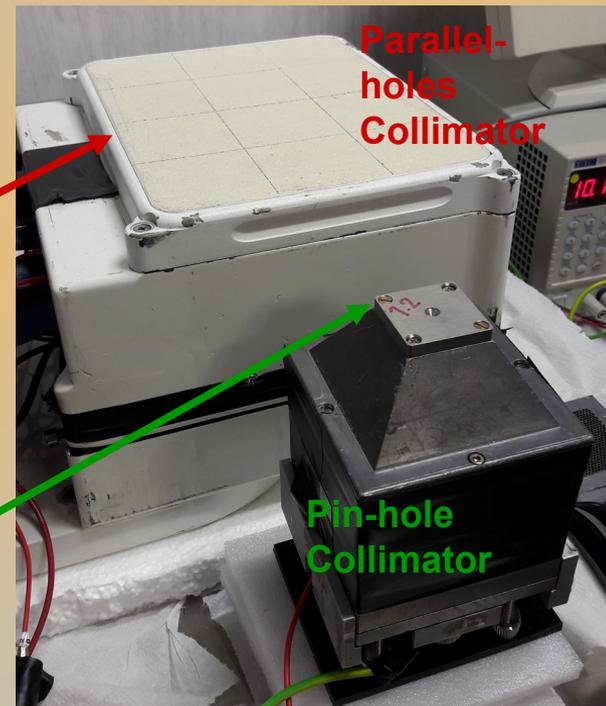
Electronics

Large Head

Small Head

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Parallel-holes Collimator

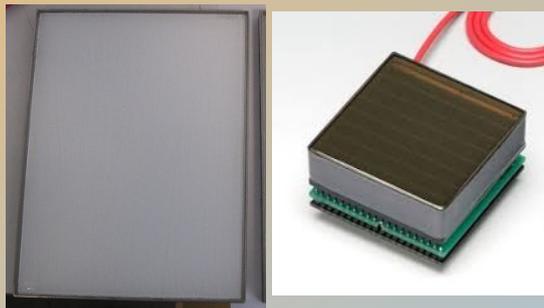
Pin-hole Collimator

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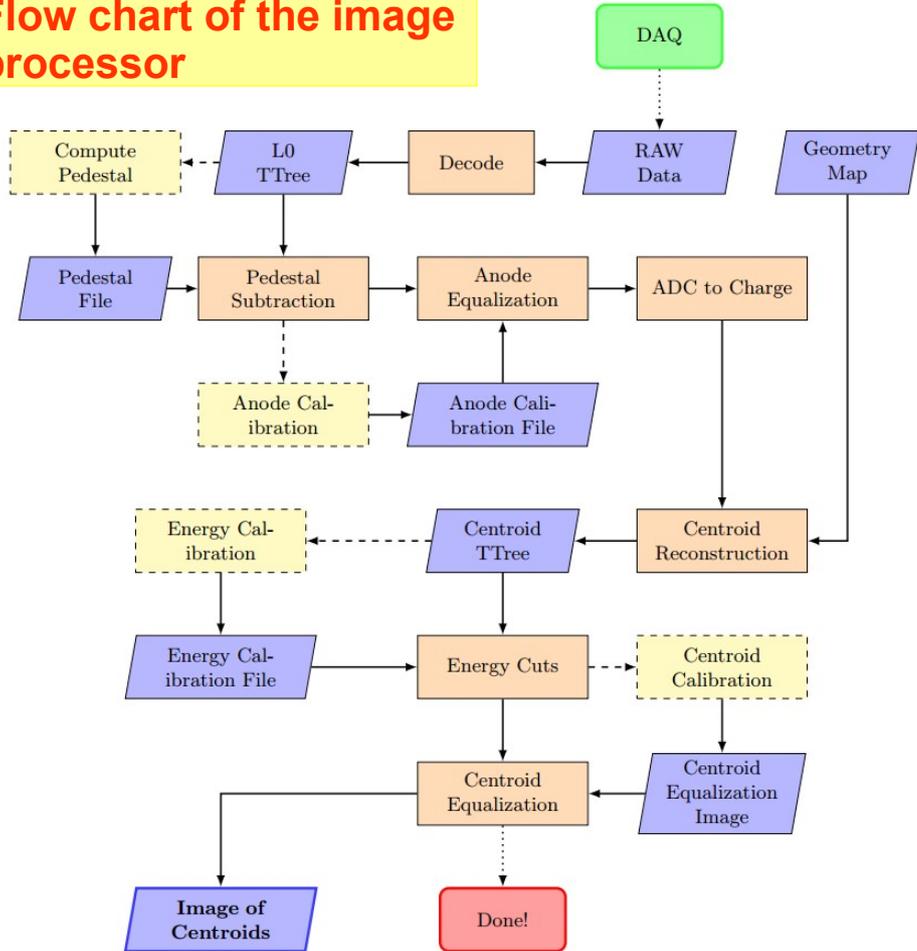
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Outlook: SiPM detectors

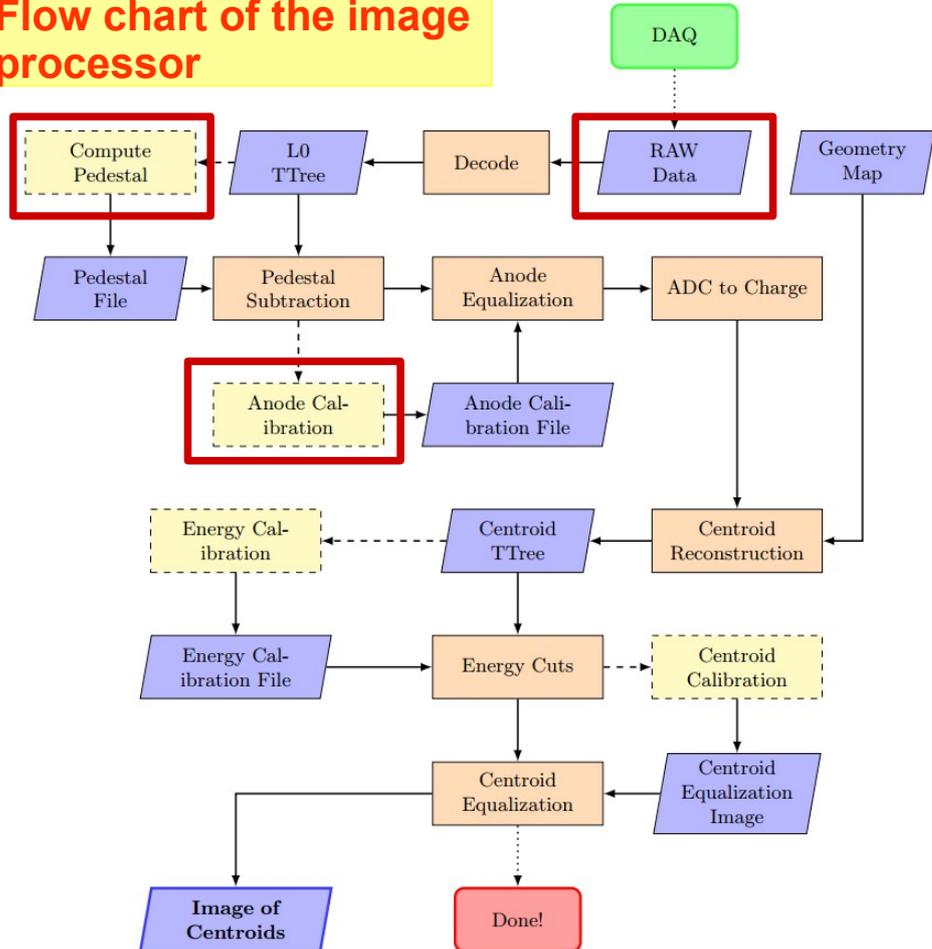
Data Processing & Image Reconstruction

Flow chart of the image processor



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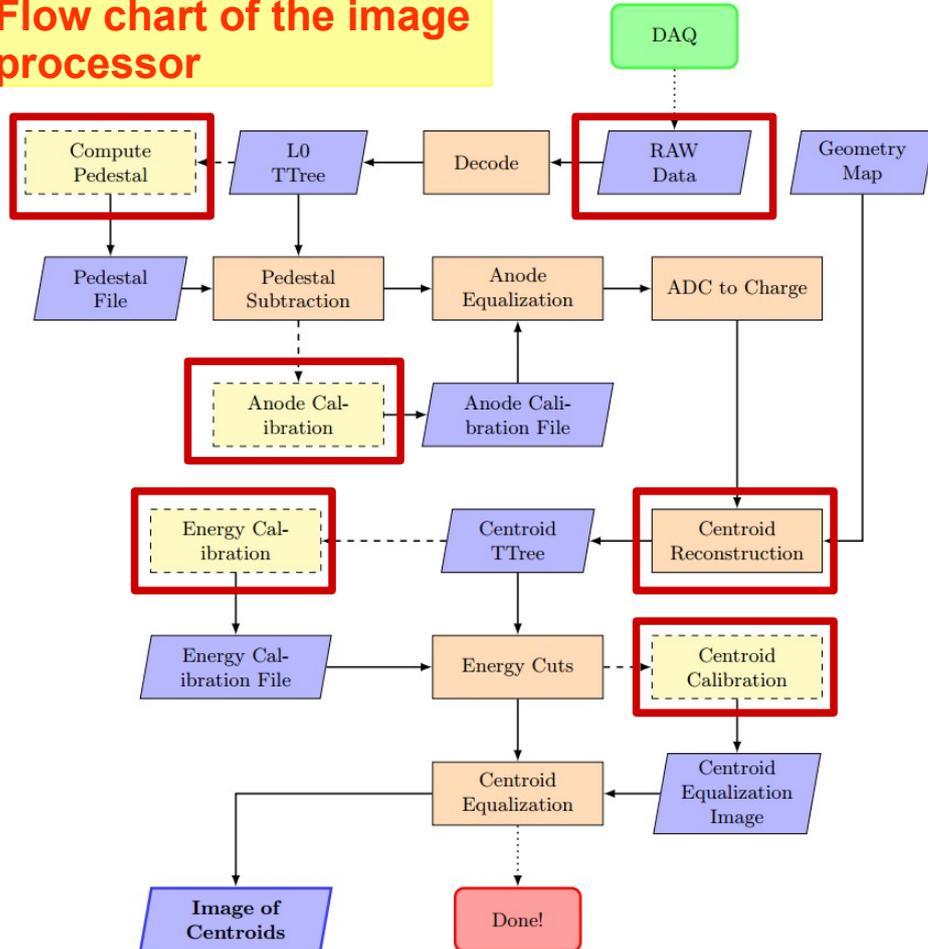
Flow chart of the image processor



- The software (C++ within the ROOT Data Analysis framework) generates the final image, from raw data, and it includes all calibrations, equalizations and corrections methods

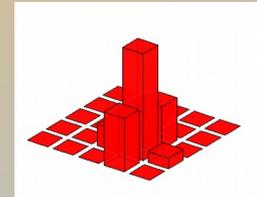
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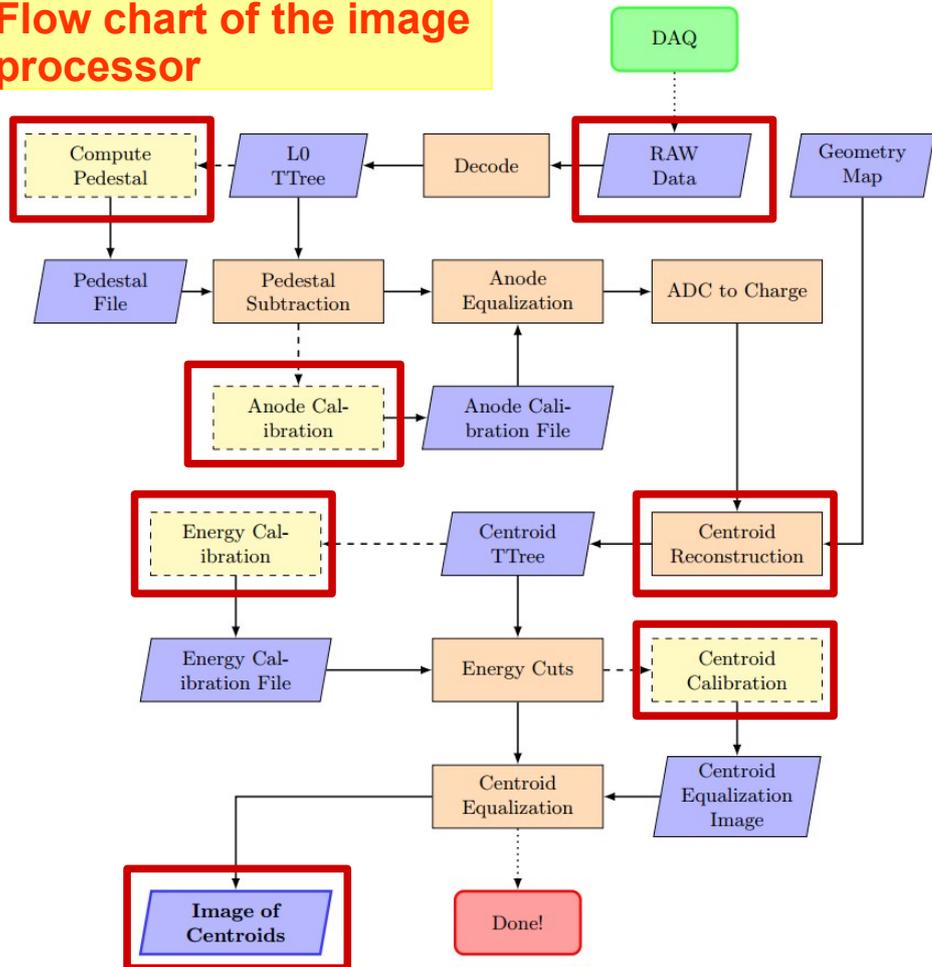
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➤ The centroid position is computed associating the count measured at the center of each photodetector



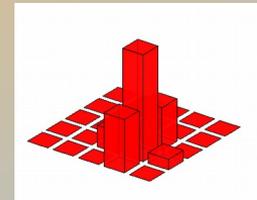
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- Final image is the image of the number of centroids in each pixel

Characterization and Calibration Campaigns

Two measurement campaigns have been performed in Rome:

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- Preparatory runs for **electronic pedestals**, **environmental bkg**, **flood** to test the uniformity response
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- Additional **scan runs** with more realistic breast phantom
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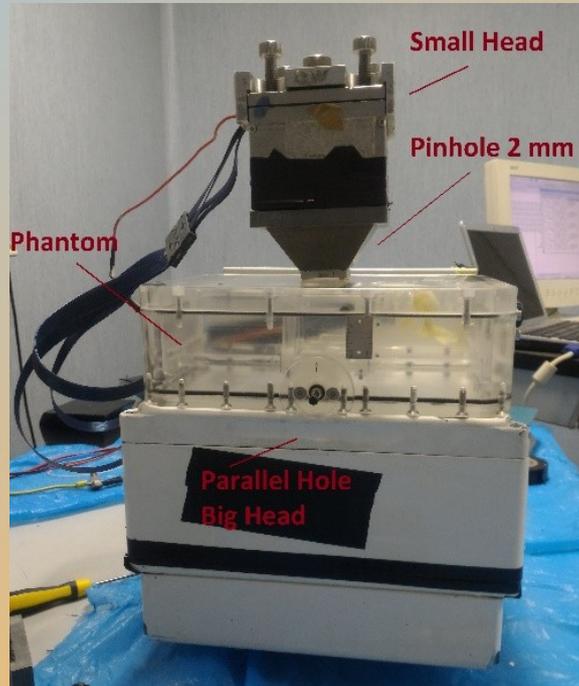
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Breast background and Tumour only can runs can be properly combined in offline analysis to get:

- Tumour uptake scan
 - Different breast sizes
- by varying the relative acquisition time

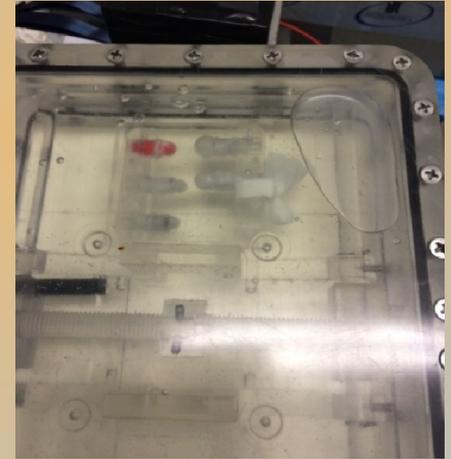
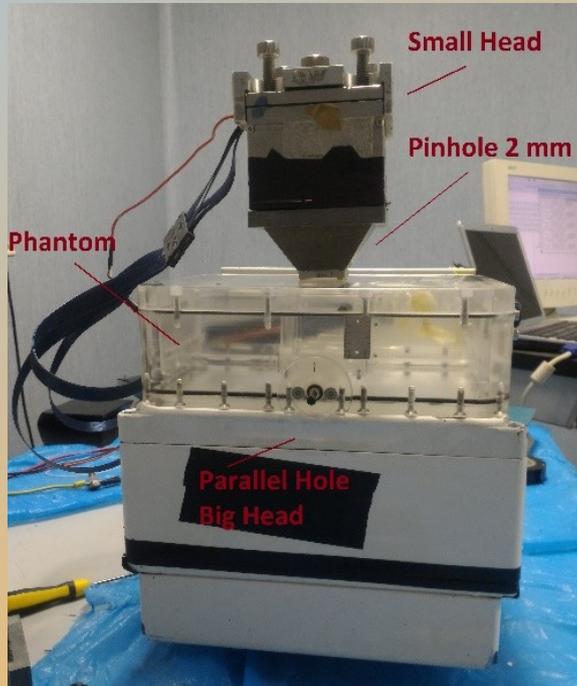
First Campaign: Experimental Setup



First Campaign: Experimental Setup

Dedicated Large Breast Phantom

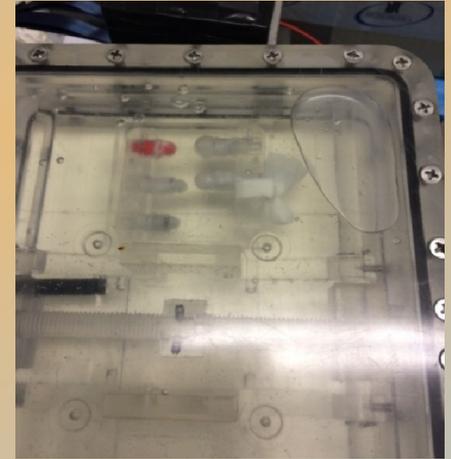
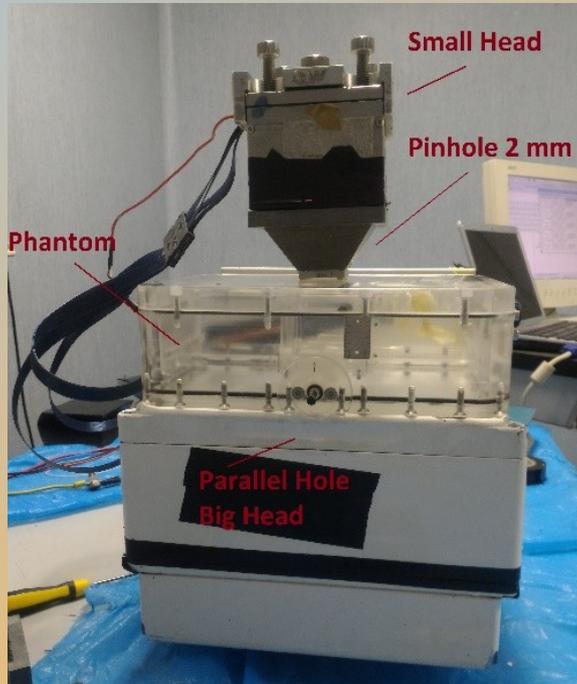
- One perspex box (20x15 cm²) filled with plain water (2l)
- Plastic support holds 5 hollow perspex spheres (tumours): 3, 4, 5, 6, 8 mm of diameter
- An internal knob allows the tumour movement, simulating different distances from the breast surface → depths inside the breast



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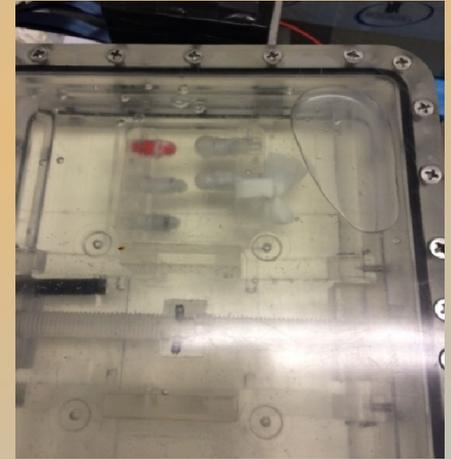
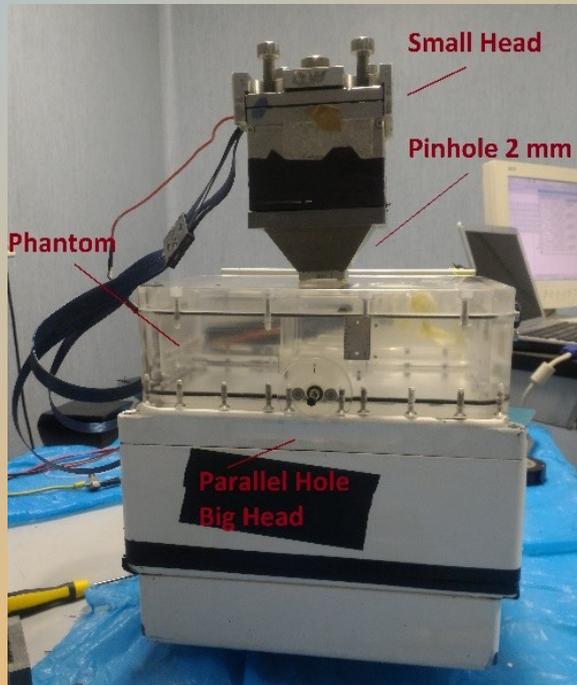
^{99m}Tc Activity and Uptake

- 740 MBq for a typical BSGI → accumulated breast activity $\approx 1\%$ ($V=1$ l)
- Breast bkg activity concentration ≈ 7 Mbq/l
- Typical Uptake in a breast lesion: 10 → Lesion Activity Concentration: 70 Mbq/l

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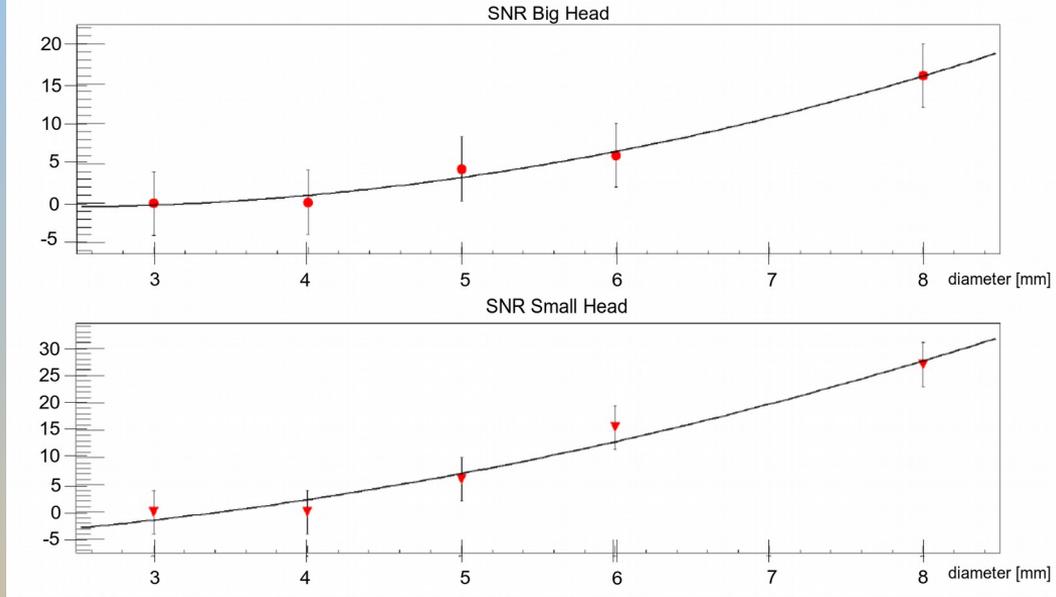
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Image Reconstruction

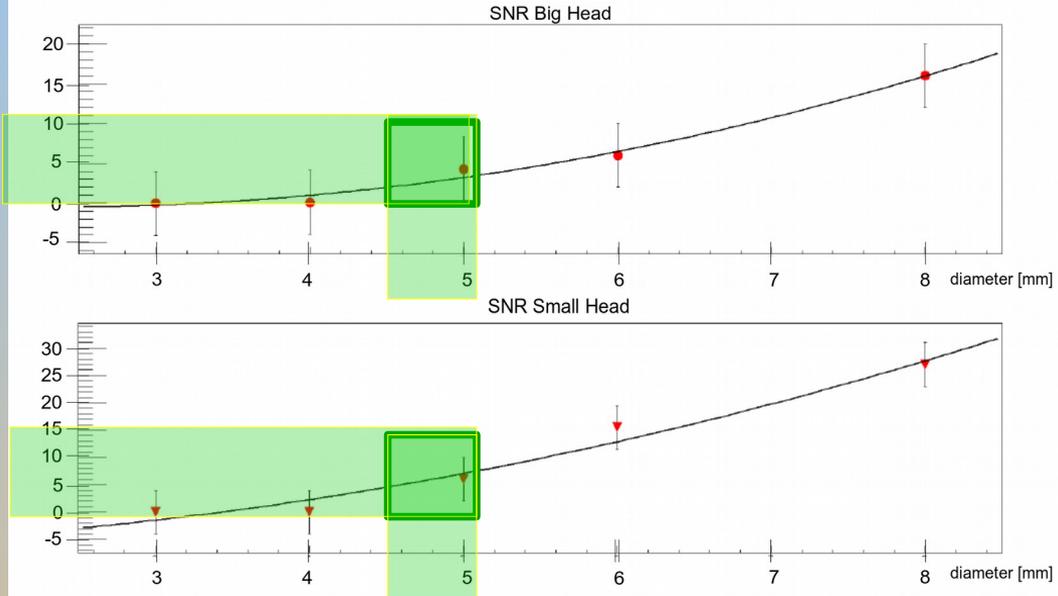
Realistic images of tumour inside breast can be obtained merging by software:

- Environmental bkg (phantom filled with plain water)
- Breast bkg (phantom filled with ^{99m}Tc water)
- Tumors (phantom filled with plain water and spheres with ^{99m}Tc saline)

Detectability and SNR

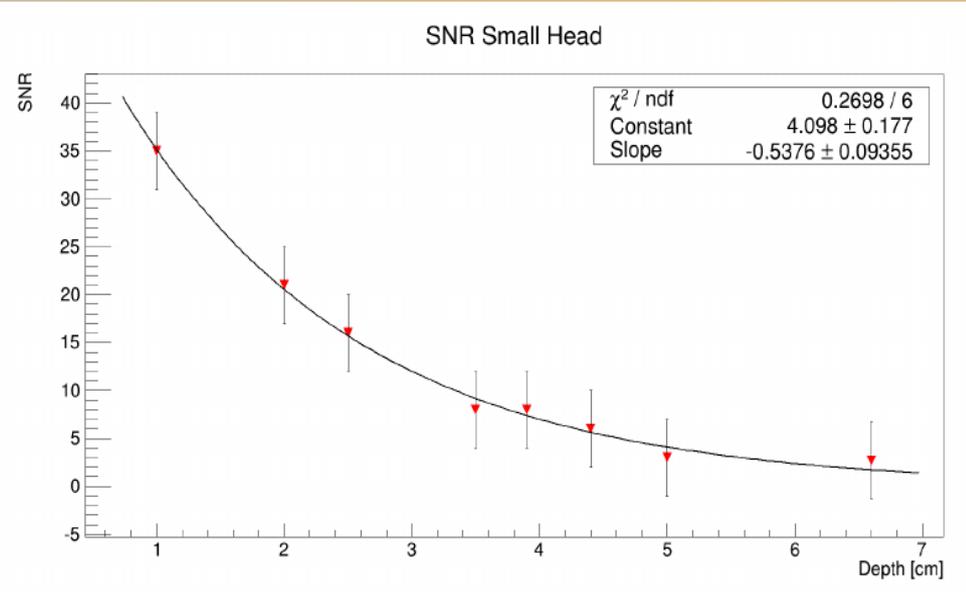
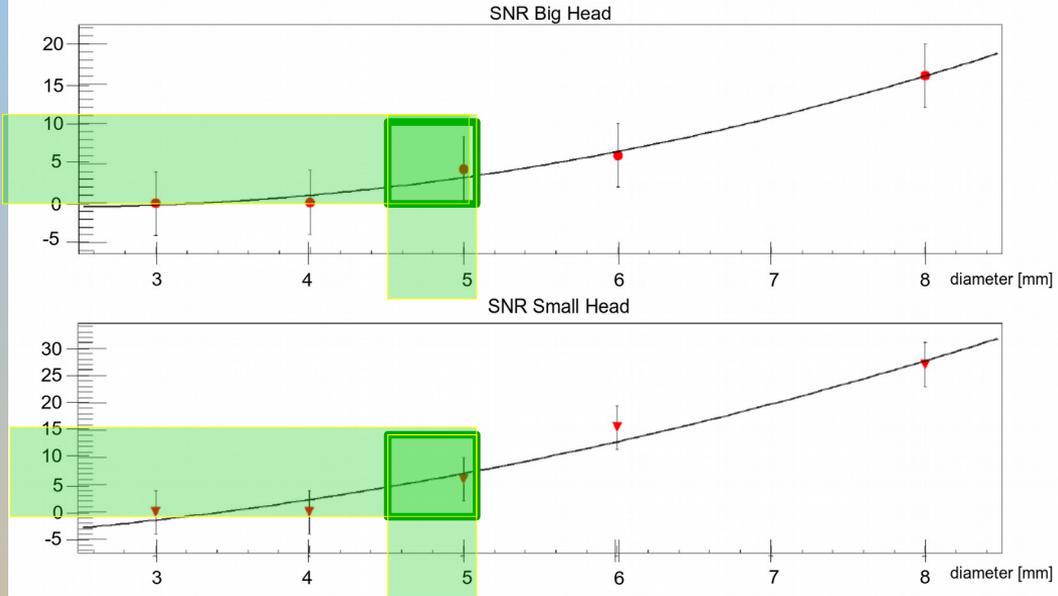


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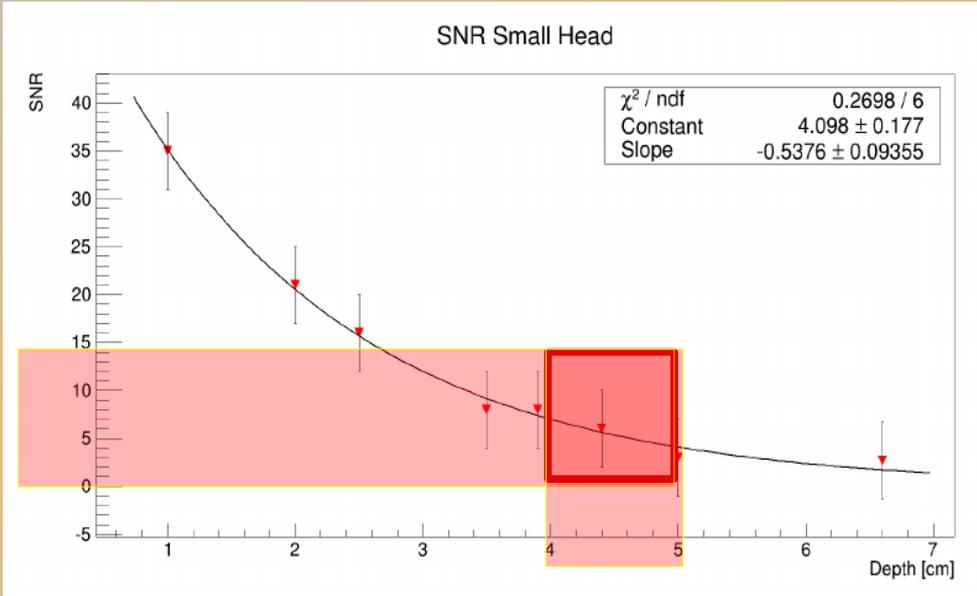
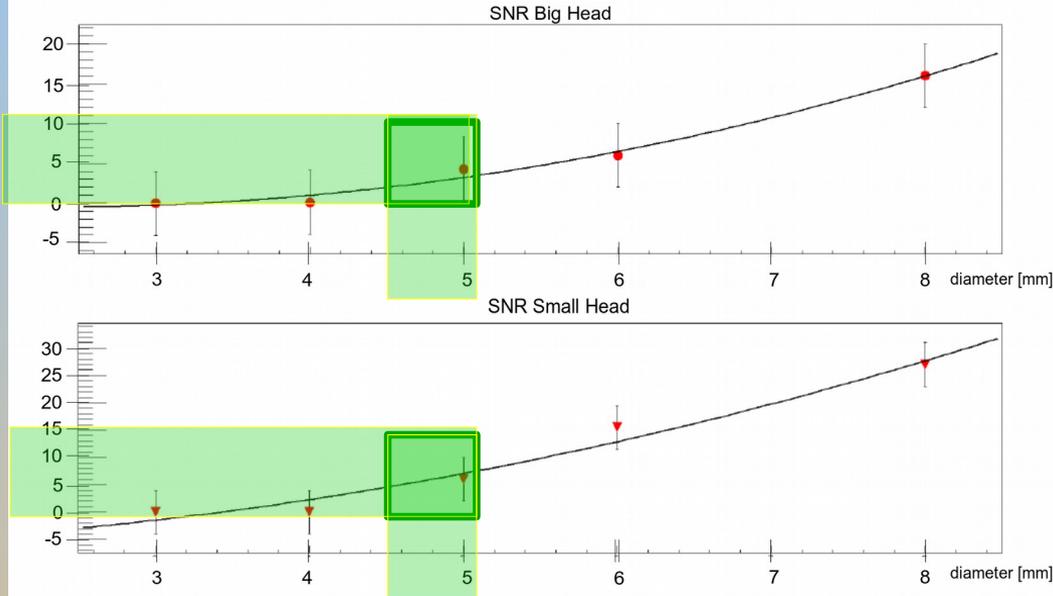
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- **The smallest visible lesion is 5 mm diameter!**

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- Fixed tumour distances of 1 cm from the Big Head and 1 cm from the Small Head
- **The smallest visible lesion is 5 mm diameter!**

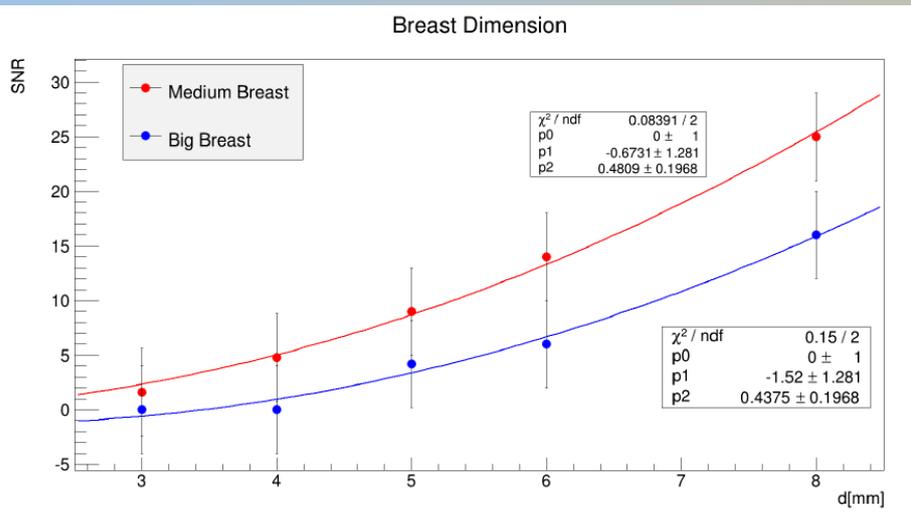
Detectability and SNR



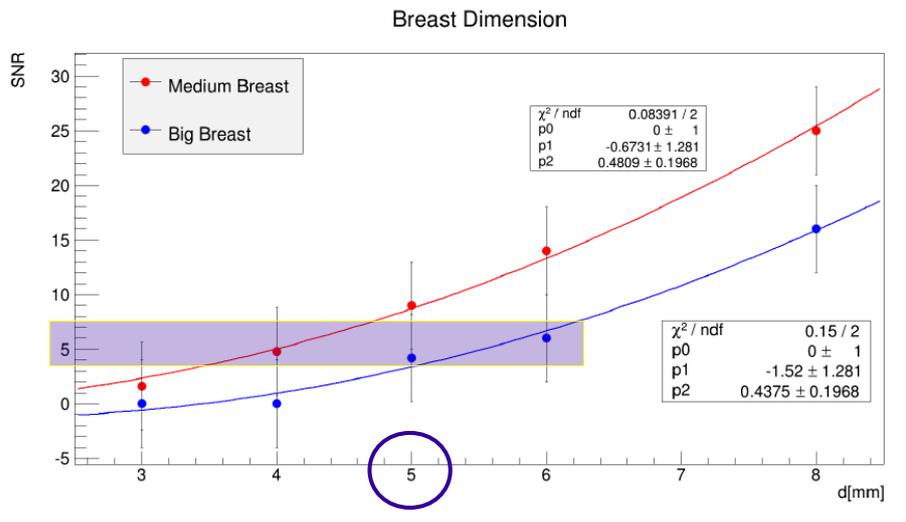
- Uptake $U=10$
- Parallel Hole collimator for both heads
- Fixed tumour distances of 1 cm from the Big Head and 1 cm from the Small Head
- **The smallest visible lesion is 5 mm diameter!**

- Uptake $U=10$
- Pinhole (reduced FOV) has been centered on 6 mm tumour
- **With the Pinhole SNR is higher than with parallel hole (fixed diameter and depth), but it decreases more rapidly**

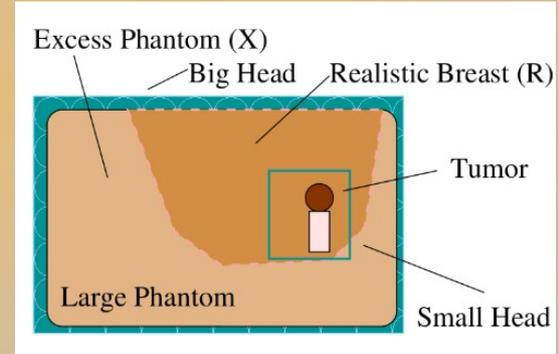
Big Head SNR versus Tumour Size & Uptake



Big Head SNR versus Tumour Size & Uptake

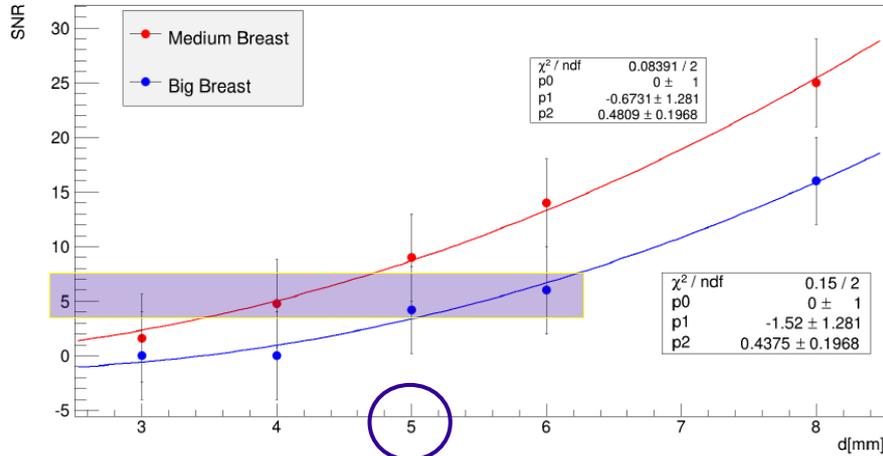


- Uptake $U=10$
- Fixed 1 cm from the Big Head
- The SNR increases of about 5, for medium tumours, moving from the full size breast phantom to half size breast

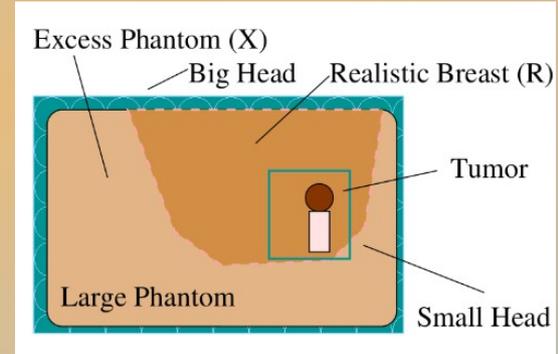


Big Head SNR versus Tumour Size & Uptake

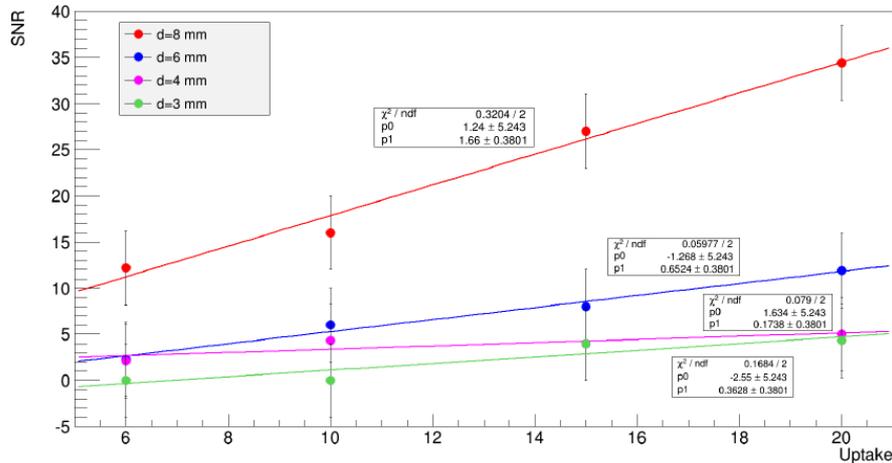
Breast Dimension



- Uptake U=10
- Fixed 1 cm from the Big Head
- The SNR increases of about 5, for medium tumours, moving from the full size breast phantom to half size breast

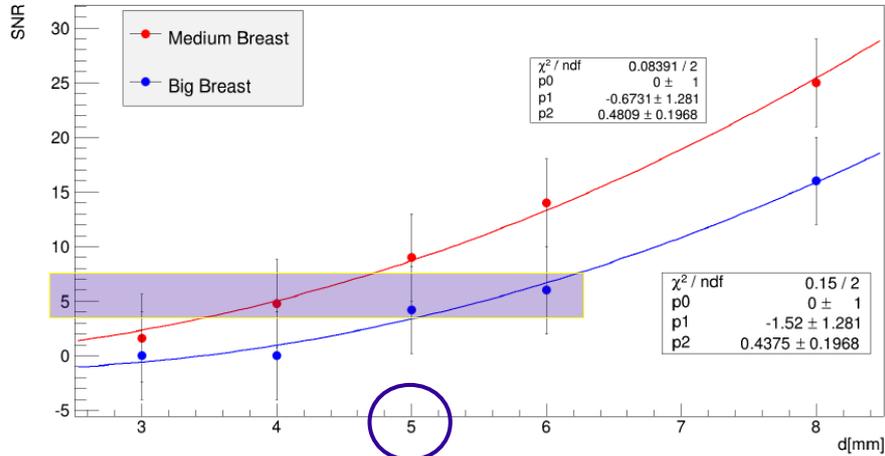


SNR vs Uptake

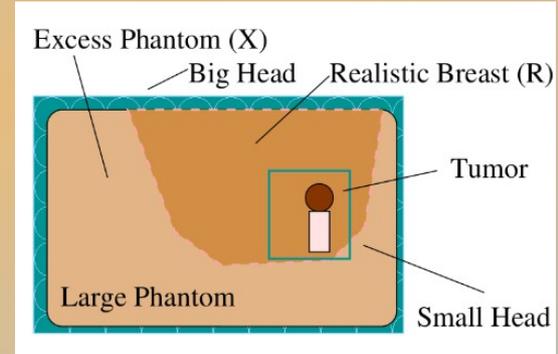


Big Head SNR versus Tumour Size & Uptake

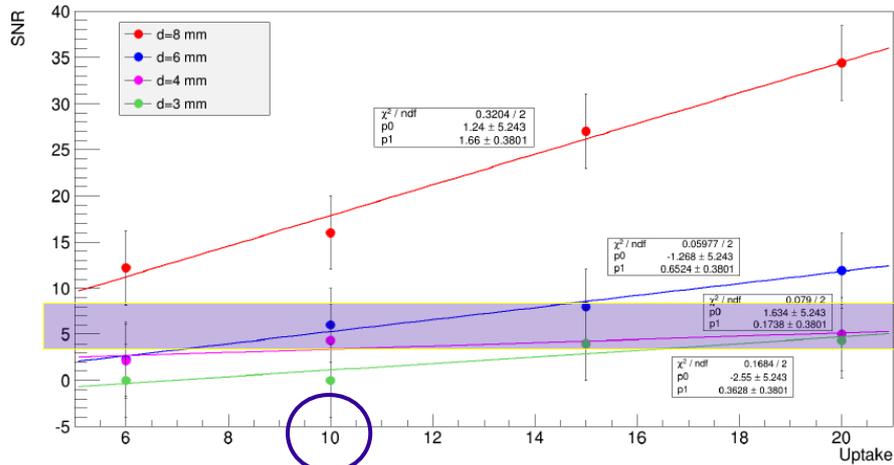
Breast Dimension



- Uptake U=10
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- The SNR increases of about 5, for medium tumours, moving from the full size breast phantom to half size breast

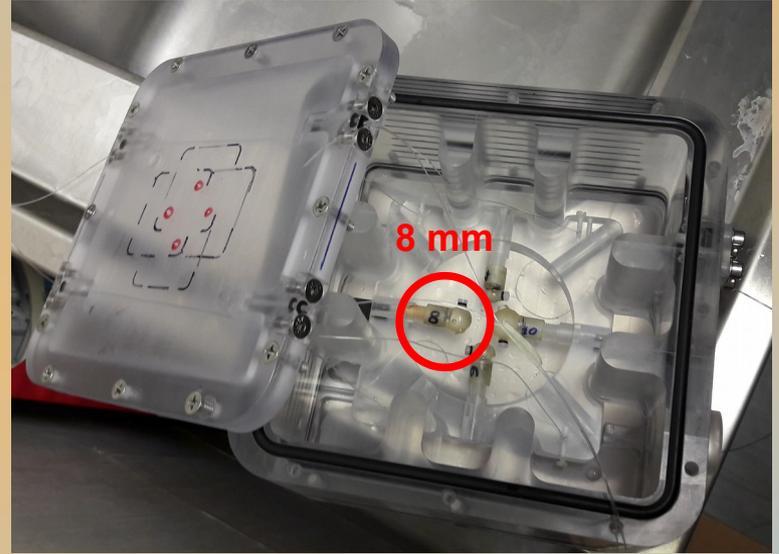
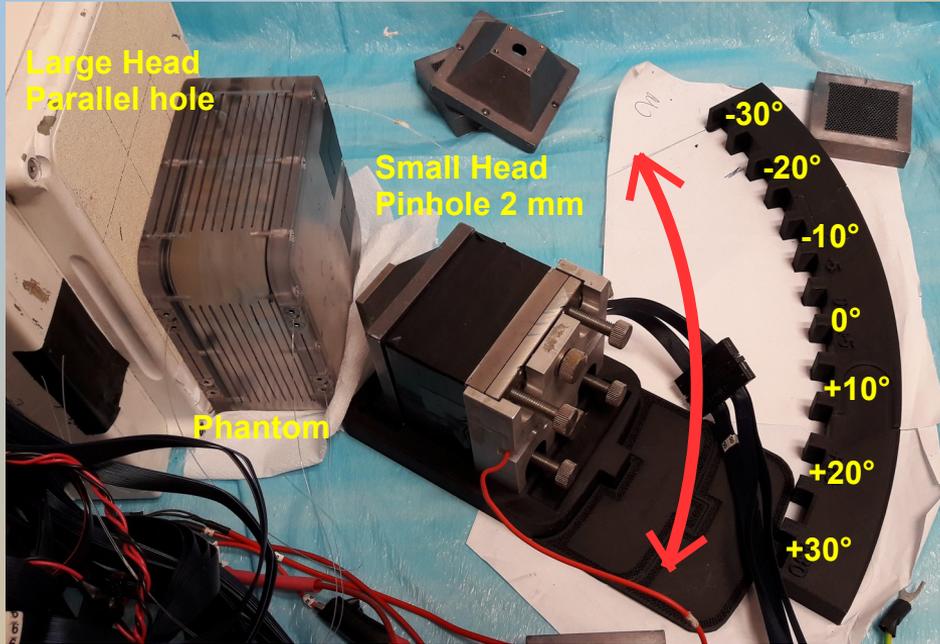


SNR vs Uptake



- Fixed 1 cm from the Big Head
- Big Breast
- Smallest tumour (3 mm diameter) becomes visible for uptake U=15
- At U=10, the SNR=5 for all the tumour sizes less than for 3 mm tumour size

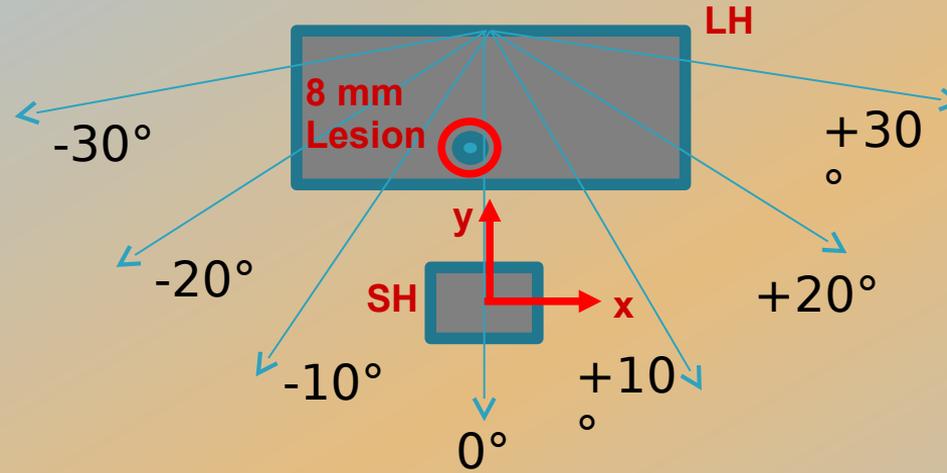
Second Campaign: LAT Experimental Setup



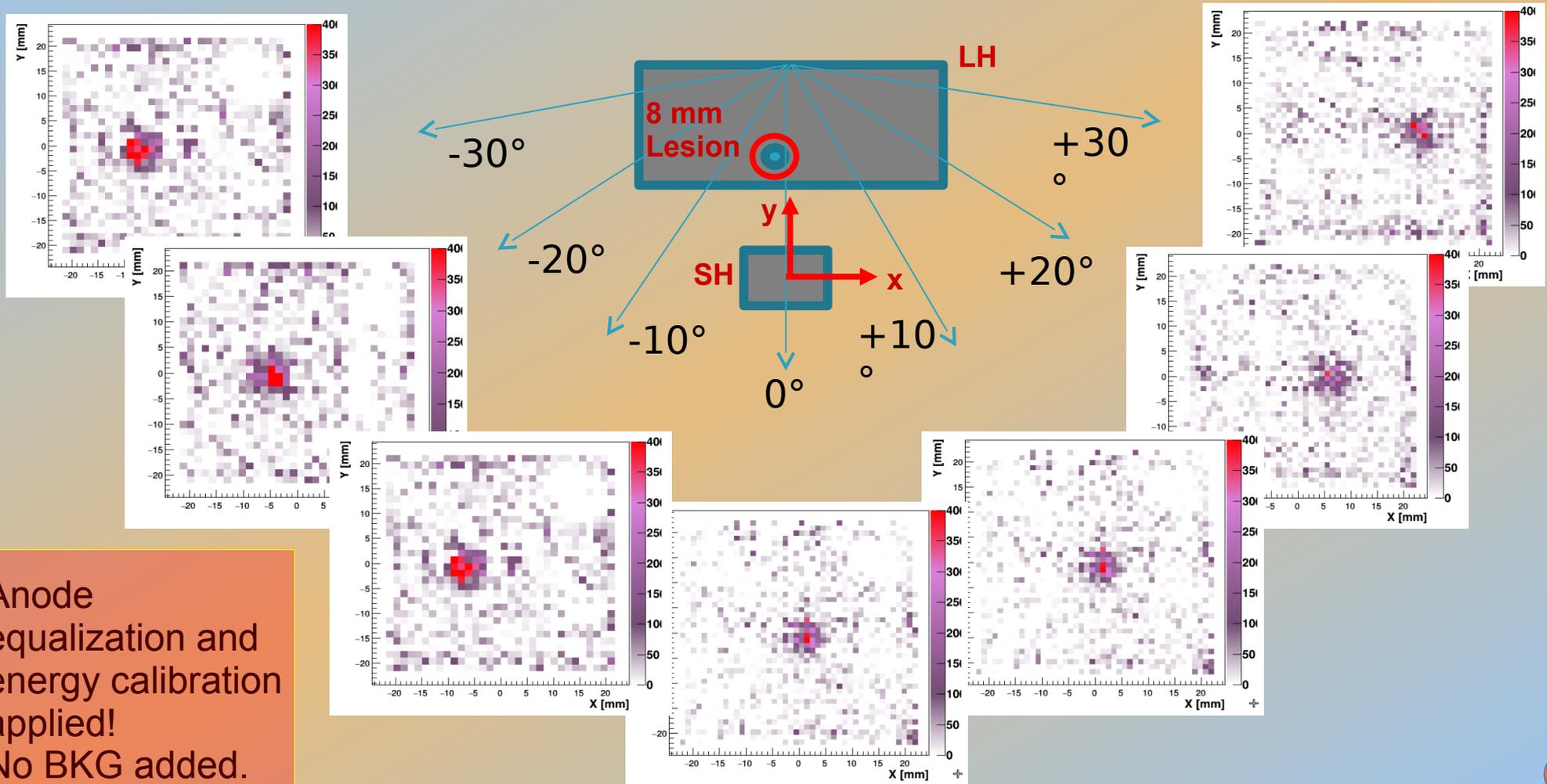
Limited Angle Tomography Configuration

- Same detector heads used in the first campaign
- New breast phantom: $10 \times 10 \times 7 \text{ cm}^3$ ($\approx 1\text{l}$, smaller than previous campaign)
- PMMA support holds up to 4 hollow perspex spheres (tumours) → **8 mm**
- Ad-hoc wires system permits to shift the tumour along the phantom thickness → **depth scan runs**

Angular Identification of Lesion by Small Head...

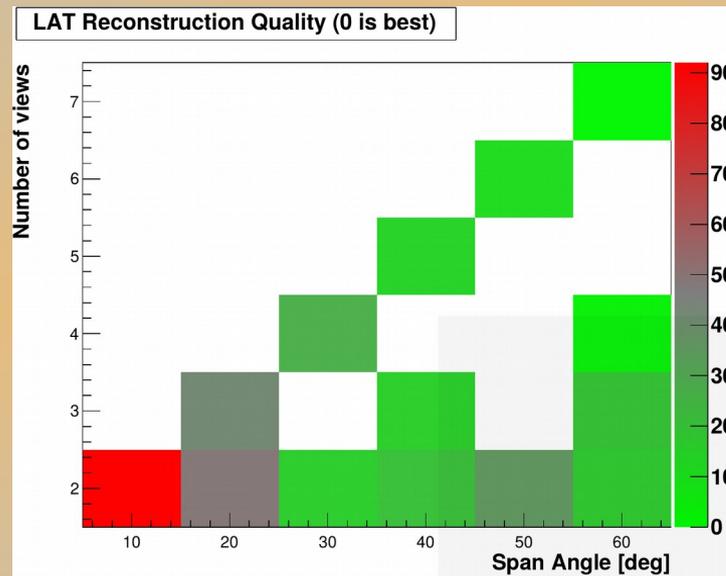
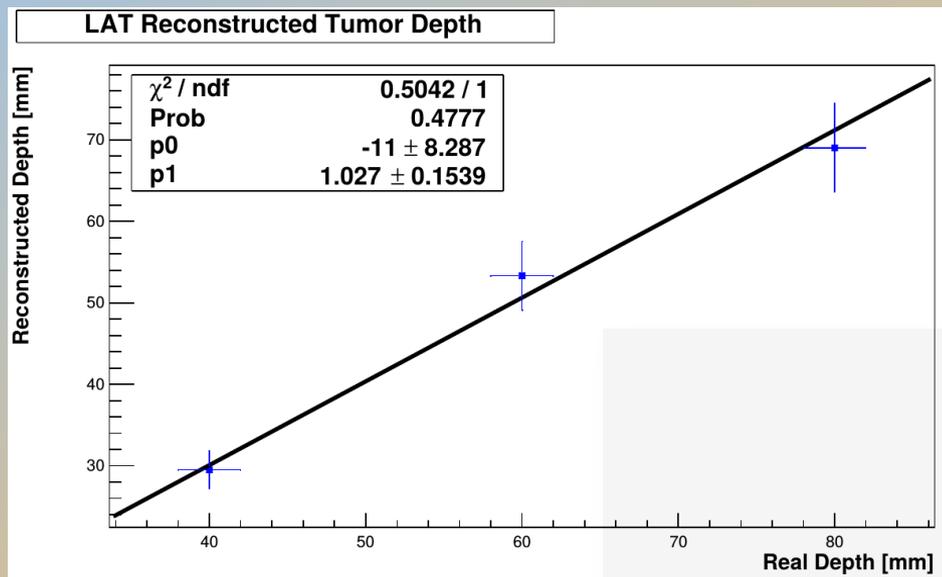


Angular Identification of Lesion by Small Head...

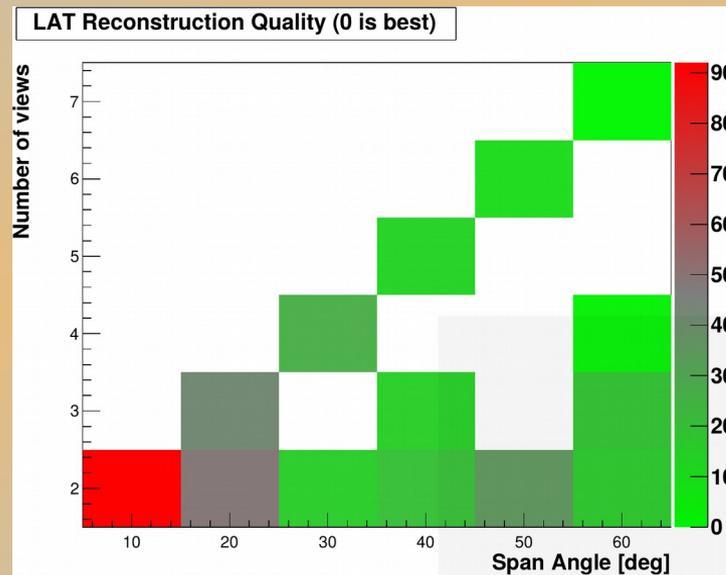
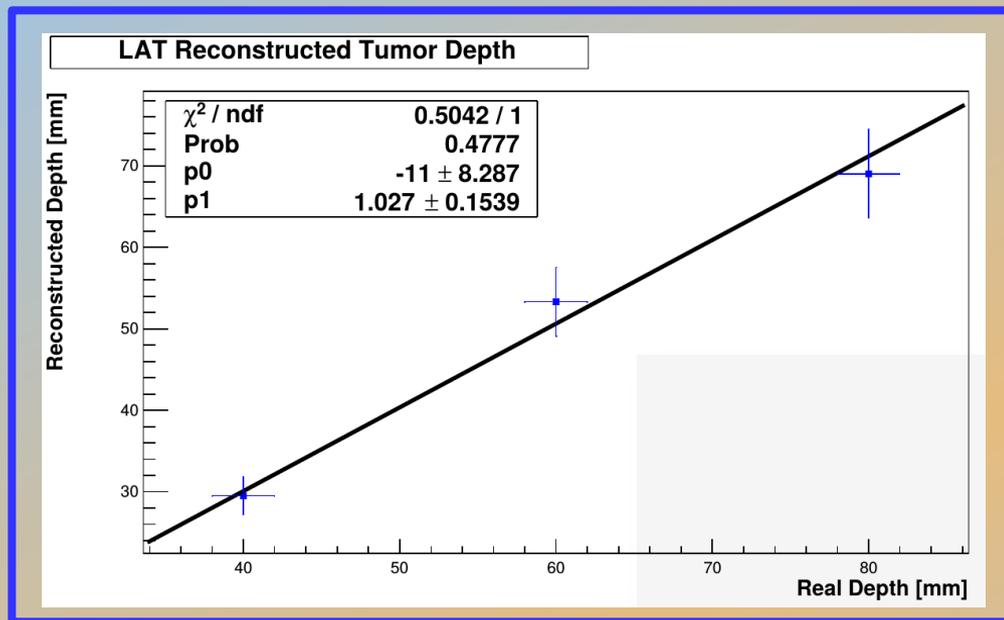


Anode
equalization and
energy calibration
applied!
No BKG added.

Deep Localization of Lesion

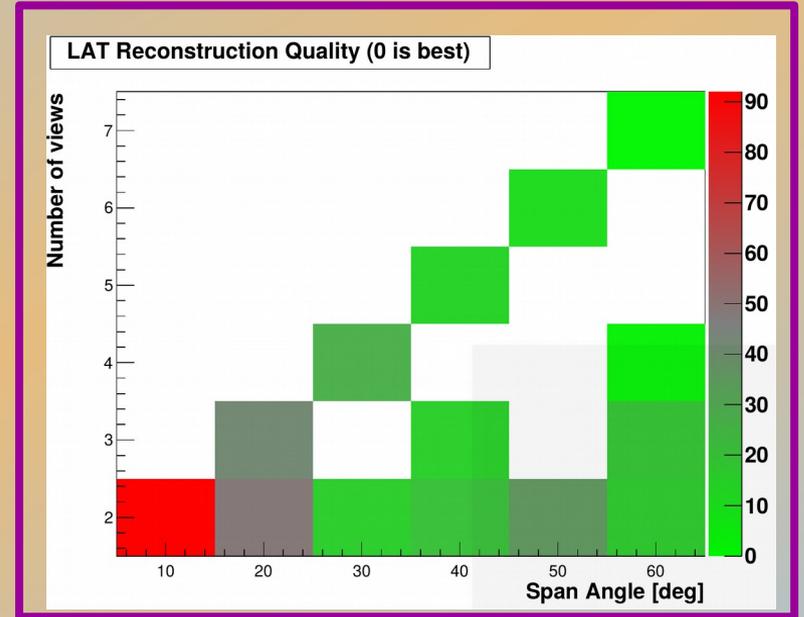
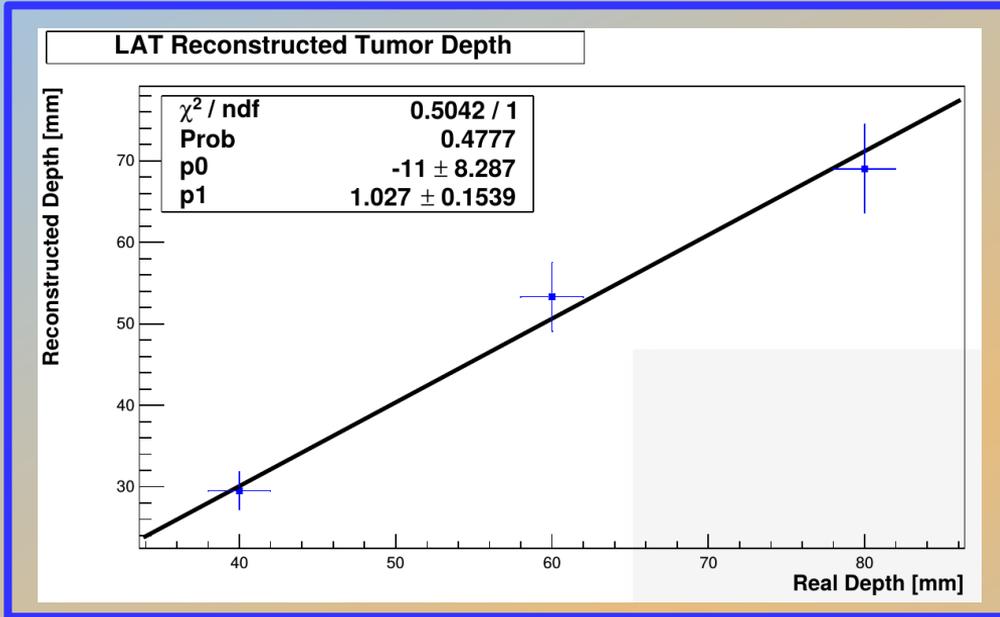


Deep Localization of Lesion



- Reconstructed versus Real Depth: span angle 60° and 7 measures for each depth (40, 60, 80 mm)
- **Result:** LAT maximum reconstruction accuracy of deep lesion \longleftrightarrow **fit slope = 1!**

Deep Localization of Lesion

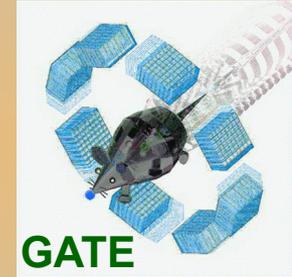


- Reconstructed versus Real Depth: span angle 60° and 7 measures for each depth (40, 60, 80 mm)
- **Result:** LAT maximum reconstruction accuracy of deep lesion \longleftrightarrow **fit slope = 1!**

- Number Of Views versus Span Angle: 7 experimental views and 60° span angle
- **Result:** LAT reconstruction quality of lesion grows with N_{VIEWS} & Span Angle

Simulation Tool

In order to improve the system performances & images optimization, a Monte Carlo simulator has been implemented in Geant4 environment, using GATE (Geant4 Application for Tomographic Emission)



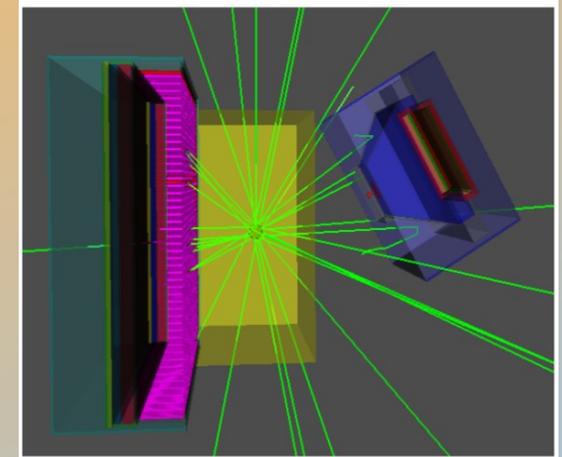
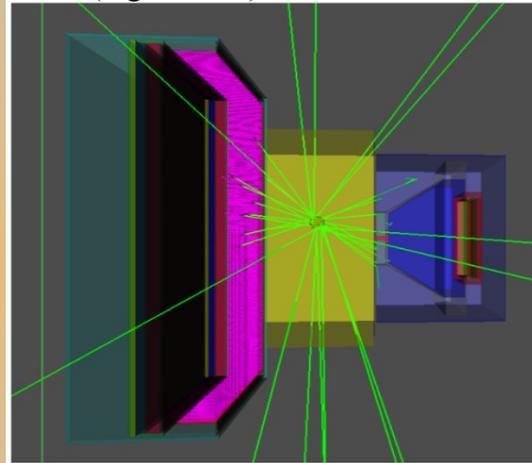
Simulation Tool

In order to improve the system performances & images optimization, a Monte Carlo simulator has been implemented in Geant4 environment, using GATE (Geant4 Application for Tomographic Emission)



SIMULATOR

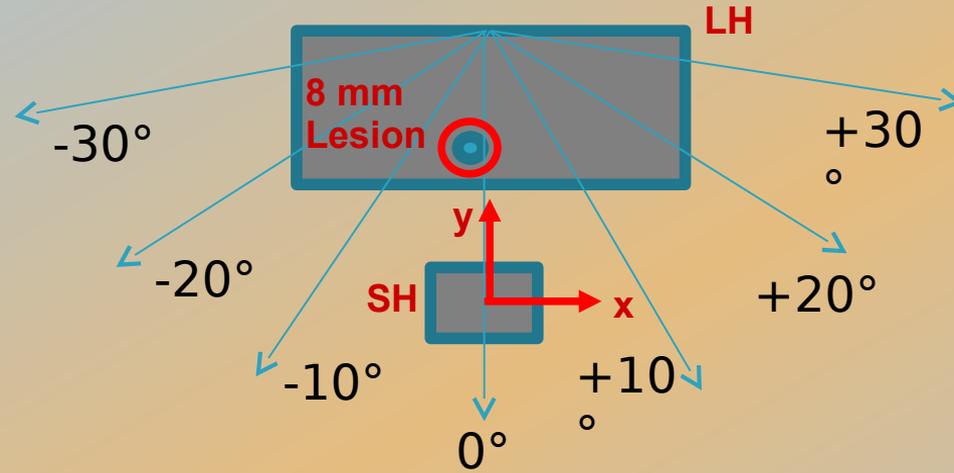
- modelisation of detectors, sources, patient
- movement (detector, patient)
- time-dependent processes (radioactive decay, movement management, biological kinetics)



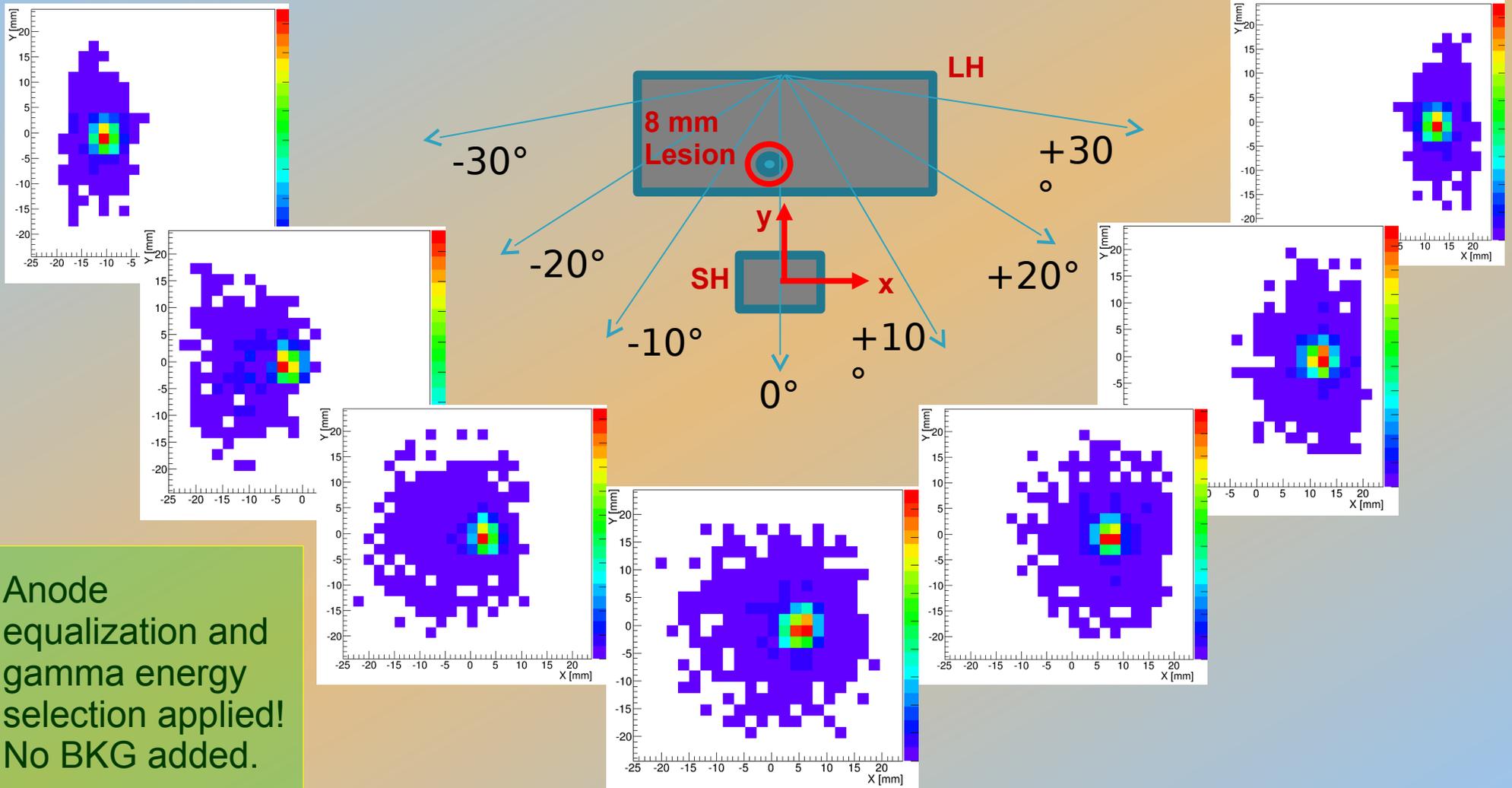
OUTLOOK

- Accurate offline analysis tool of raw data in output from the Monte Carlo simulation
- Optimization of reconstruction algorithms
- Definition of acquisition protocols
- System configuration evaluation to improve the lesion detectability & quantification, Image corrections

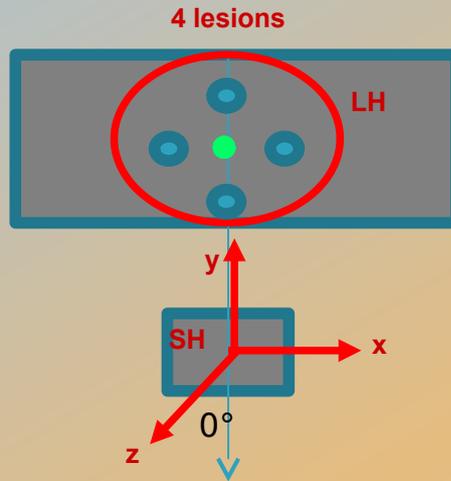
...Angular Identification: GATE simulations



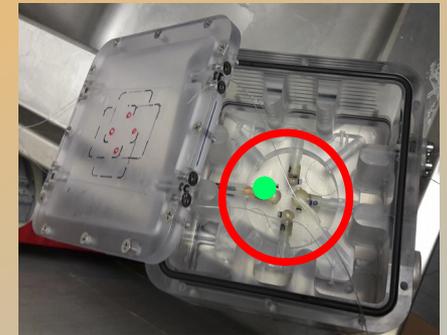
...Angular Identification: GATE simulations



Second Campaign: Spot-Compression Experimental Setup



BREAST PHANTOM: 4 lesions



Spot-Compression Configuration

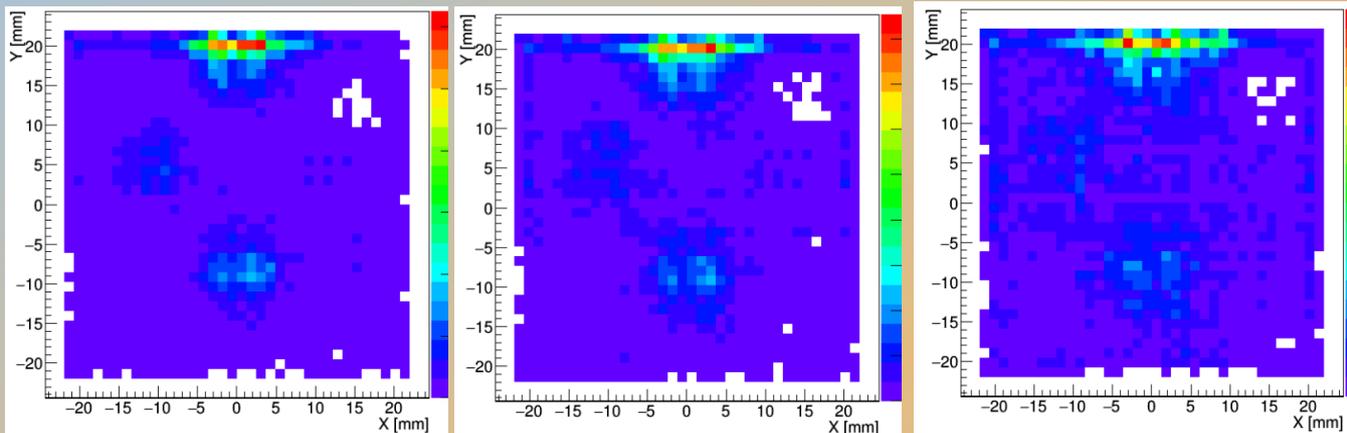
- Same detector heads and breast phantom used in the LAT experimental setup, 3 lesion depths investigated
- SH head with parallel-holes (pinhole) collimator → centered to the center of 4 lesions (8 mm lesion)

^{99m}Tc Activity and Uptake

- Breast bkg activity concentration ≈ 5 Mbq/l
- Typical Uptake in a breast lesion: 6 (10) → Lesion Activity Concentration: 30 (50) KBq/ml

Spot Compression Configuration: Parallel-holes Collimator

Real Data

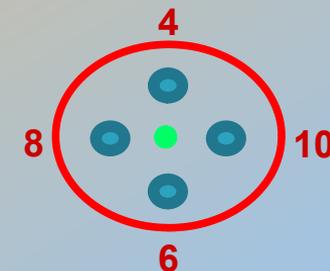
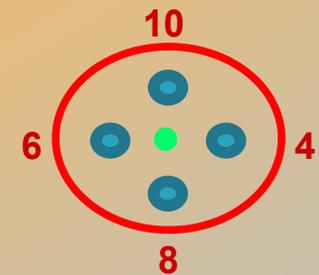
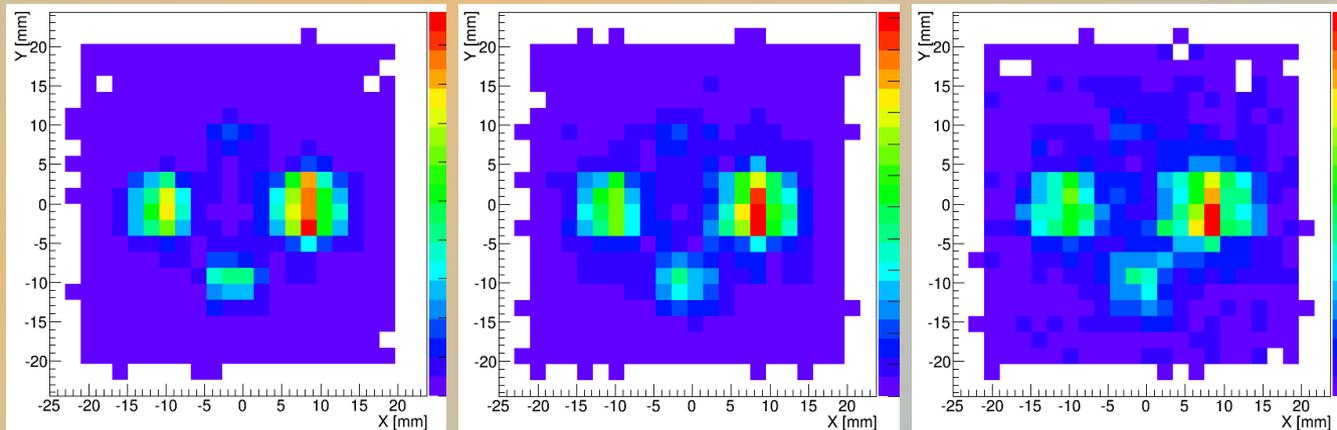


Lesions close to SH

Lesions in middle

Lesions close to LH

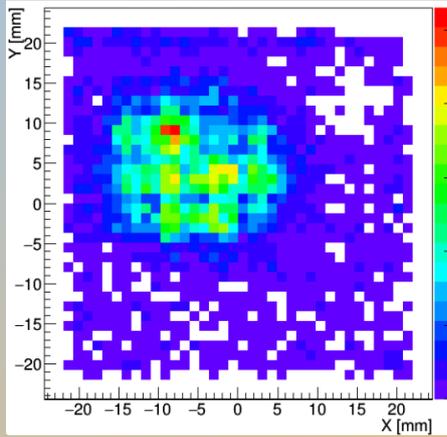
Simulated Data



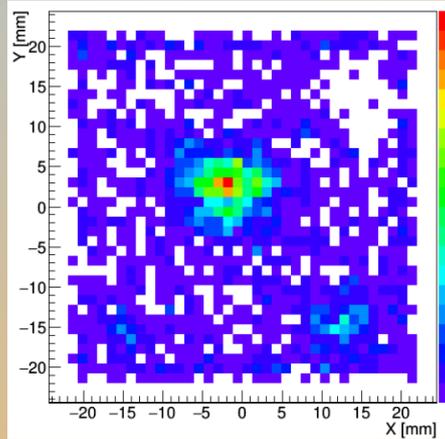
Spot Compression Configuration: Pin-hole Collimator

Real Data

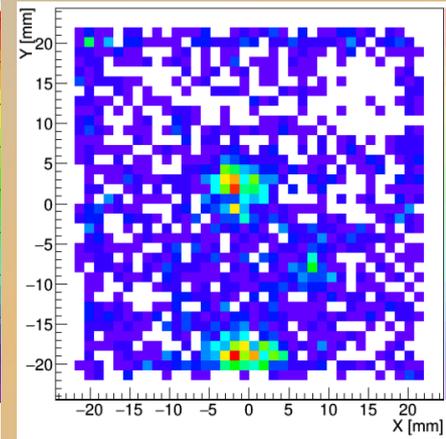
→ 8 mm



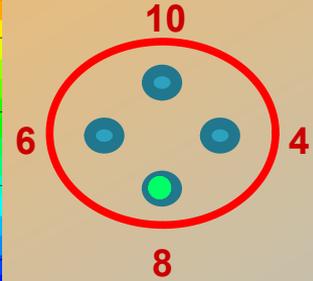
Lesions close to SH



Lesions in middle

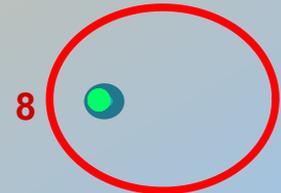
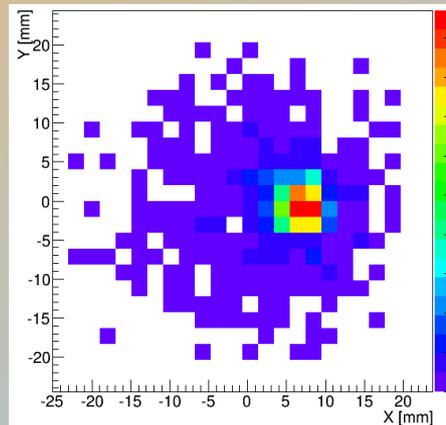
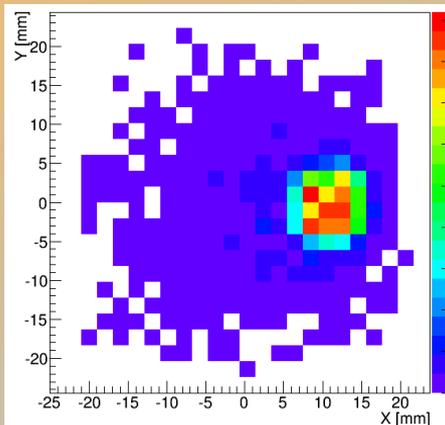
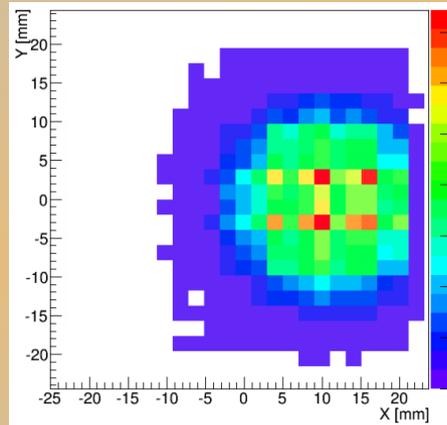


Lesions close to LH



Simulated Data

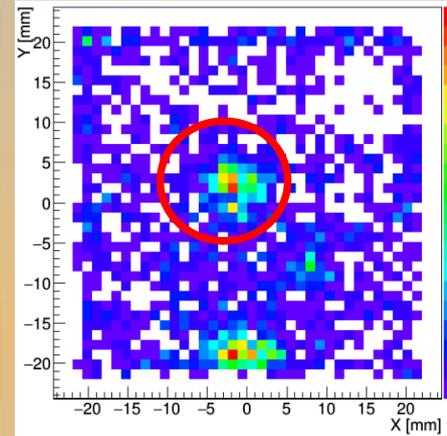
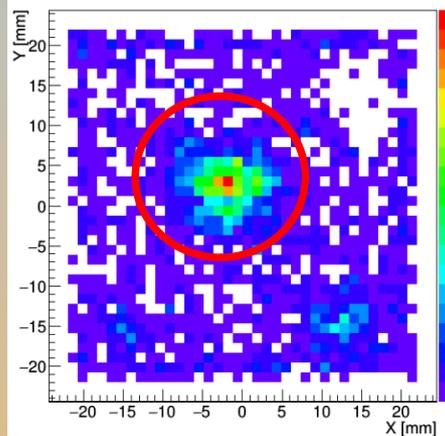
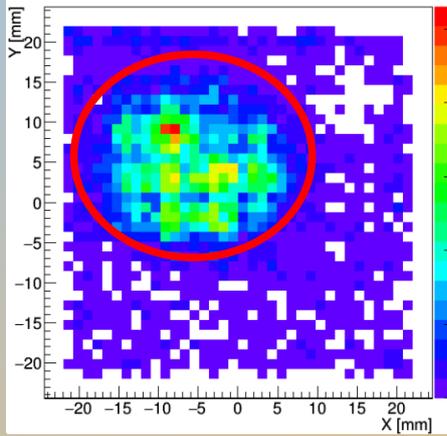
→ 8 mm



Spot Compression Configuration: Pin-hole Collimator

Real Data

→ 8 mm



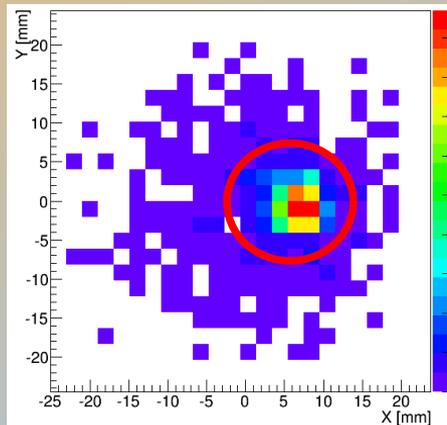
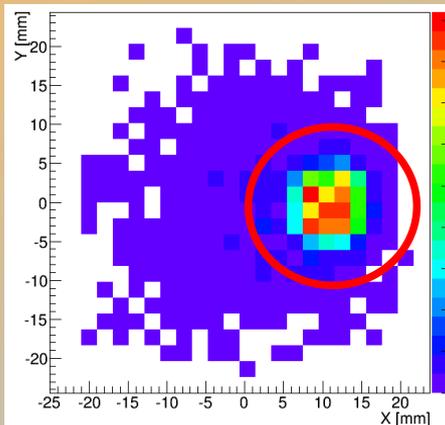
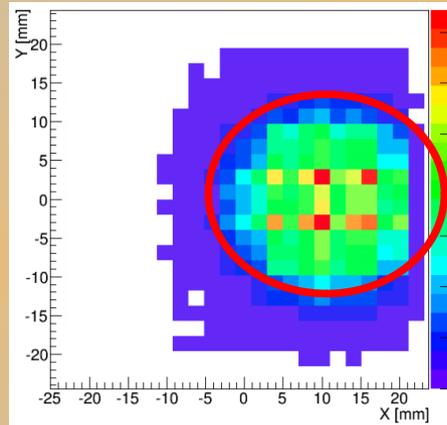
Lesions close to SH

Lesions in middle

Lesions close to LH

Simulated Data

→ 8 mm



Conclusion & Outlook

- Development of new dedicated dual-asymmetrical head compact Gamma Camera is under calibration and characterization to improve the detection sensitivity for sub cm lesions
- The quality of reconstructed images has been optimized with deep calibration and characterization, and accurate data processing
- First results on lesion detectability shows approx. 5 mm diameter as lower limit (with nominal Uptake = 10)
- Preliminary analysis on limited angle tomography:
 - good correspondence of reconstructed and real tumour depth (in optimal conditions)
 - reconstruction improves with larger span angle and number of views (as expected); but trade off between them and clinical session time and complexity need to be evaluated
- Reliability of GATE simulations and the fusion of BKG and lesion images will allow to find the best configuration to detect the cancers lesions smaller than 5 mm using an Uptake < 10
- Analysis will be continued and integrated by simulations: images fusion in 2D and 3D
- New measurements on LAT will overcome current limitations on mechanical accuracy of the heads positioning

**THANKS FOR YOUR
ATTENTION**

Email: elio.poma@ct.infn.it